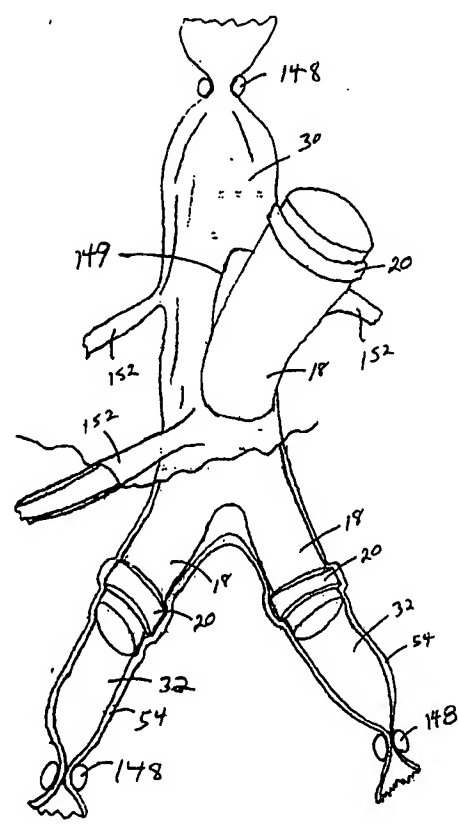




INTERNATIONAL APPLICATION PUBLISHED UNDER THE PATENT COOPERATION TREATY (PCT)

<p>(51) International Patent Classification ⁶ : A61F 2/06</p>	<p>A1</p>	<p>(11) International Publication Number: WO 00/15144 (43) International Publication Date: 23 March 2000 (23.03.00)</p>
<p>(21) International Application Number: PCT/US99/13189 (22) International Filing Date: 10 June 1999 (10.06.99) (30) Priority Data: 60/088,705 10 June 1998 (10.06.98) US 60/111,948 11 December 1998 (11.12.98) US (71) Applicant: ADVANCED BYPASS TECHNOLOGIES, INC. [US/US]; 7026 Koll Center Parkway, Suite 230, Pleasanton, CA 94566 (US). (72) Inventors: HOUSER, Russell, A.; 1787 Verdite Street, Liv- ermore, CA 94550 (US). WHAYNE, James, G.; 868 Del Avion Lane, San Jose, CA 95138 (US). FLEISCHMAN, Sidney, D.; 855 Woodland Avenue, Menlo Park, CA 94025 (US). (74) Agent: REVELOS, William, C.; Morrison & Foerster LLP, 755 Page Mill Road, Palo Alto, CA 94304-1018 (US).</p>		<p>(81) Designated States: AU, JP, European patent (AT, BE, CH, CY, DE, DK, ES, FI, FR, GB, GR, IE, IT, LU, MC, NL, PT, SE). Published <i>With international search report.</i></p>
<p>(54) Title: AORTIC ANEURYSM TREATMENT SYSTEMS</p> <p>(57) Abstract</p> <p>A system, and components for treating aortic aneurysms includes a reinforcing graft (18), fittings (20) for securing the graft to a host vessel, to branch vessels, for example the iliac, and renal arteries. Combinations of fittings (20), and rings (22) or other compression mechanisms secure vessels or grafts frictionally, for end to end (20) or end side couplings. A variety of tools (38, 42) are disclosed for manipulating retaining rings (22), everting portions of grafts (18) or vessels in the course of coupling them to fittings (20), and clamping fittings (20) while positioning the retaining rings (22).</p> 		

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AORTIC ANEURYSM TREATMENT SYSTEMS

This application claims the benefit of Provisional Application No. 60/088,705 entitled
5 “Bypass Graft Mechanical Securing Systems” filed June 10, 1998, and Provisional Application
No. 60/111,948 entitled “Bypass Graft Positioning and Securing Systems” filed December 11,
1998.

Background of the Invention

10 This invention relates to devices and processes for treating aortic aneurysms
(abdominal aortic aneurysms, thoracic aortic aneurysms, and thoracoabdominal aortic
aneurysms). More particularly, the invention relates to devices and techniques for securing a
graft to reinforce the aorta and reattach branching vessels that would otherwise be occluded. In
addition, the invention addresses other treatment modalities involving reattaching branching
15 vessels to the reinforcing graft. These include aortic root replacements for aortic dissections in
which the left and right coronary arteries must be reattached to the replacement graft, and
extracranial carotid aneurysm repair involving reattaching the internal carotid artery and/or the
external carotid artery to a replacement graft. More particularly, this invention applies to all
aneurysm treatment regimens involving attaching a reinforcing graft or replacement graft to
20 isolate or remove the aneurysm and reattach branching vessels that would otherwise be
occluded or separated. Embodiments of the invention enable rapidly securing grafts to the
vasculature without the need to suture the graft to the host vessel wall, or to stop or re-route
blood flow through the host vessel to reattach branching vessels.

Current techniques for producing anastomoses during aortic aneurysm procedures
25 involve interrupting blood flow for a prolonged period of time to suture, clip, or staple a graft
to the aorta. Interrupting blood flow is associated with substantial morbidity and mortality.
Less invasive attempts at treating aortic aneurysms involve percutaneously deploying grafts
into the abdominal aorta or thoracic aorta and securing the grafts with hooks or stents. Most of
these less invasive approaches occlude blood flow while balloon catheters are used to position

and expand the securing components into contact with the vessel. In addition, these approaches do not address branching vessels that can be occluded when grafts extend past the branching vessels to isolate the aneurysm from blood flow.

Attempts to automate formation of sutureless anastomoses have led to mechanical stapling devices. Mechanical stapling devices have been proposed for creating end-end anastomoses between the open ends of transected vessels. Berggren, et al propose an automatic stapling device for use in microsurgery (U.S. Patents 4,607,637; 4,624,257; 4,917,090; 4,917,091). This stapling device has mating sections containing pins that are locked together after the vessel ends are fed through lumens in the sections and everted over the pins. This stapling device maintains intima to intima apposition for the severed vessel ends but has a large profile and requires impaling the everted vessel wall with the pins. Sakura describes a mechanical end-end stapling device designed to reattach severed vessels (U.S. Patent 4,214,587). This device has a wire wound into a zig-zag pattern to permit radial motion and contains pins bonded to the wire that are used to penetrate tissue. One vessel end is everted over and secured to the pins of the end-end stapling device, and the other vessel end is advanced over the end-end stapling device and attached with the pins. Sauer, et al proposes another mechanical end-end device that inserts mating pieces into each open end of a severed vessel (U.S. Patent 5,503,635). Once positioned, the mating pieces snap together thereby bonding the vessel ends. These end-end devices are amenable to reattaching severed vessels but are not suitable to producing end-end anastomoses between a graft and an intact vessel, especially when exposure to the vessel is limited.

Mechanical stapling devices have also been proposed for end-side anastomoses. These devices are designed to insert bypass grafts, attached to the mechanical devices, into the host vessel through a large incision and secure the bypass graft to the host vessel. Kaster describes vascular stapling apparatus for producing end-side anastomoses (U.S. Patents 4,366,819; 4,368,736; and 5,234,447). Kaster's end-side apparatus is inserted through a large incision in the host vessel wall. The apparatus has an inner flange that is placed against the interior of the

vessel wall, and a locking ring that is affixed to the fitting and contains spikes that penetrate into the vessel thereby securing the apparatus to the vessel wall. The bypass graft is itself secured to the apparatus in the everted or non-everted position through the use of spikes incorporated in the apparatus design.

5 U.S. Surgical has developed automatic clip appliers that replace suture stitches with clips (U.S. Patents 5,868,761; 5,868,759; 5,779,718). These clipping devices have been demonstrated to reduce the time required when producing the anastomosis but still involve making a large incision through the host vessel wall. As a result, blood flow through the host vessel must be interrupted while creating the anastomoses.

10 Gifford, et al provides end-side stapling devices (U.S. Patent 5,695,504) that secure harvested vessels to host vessel walls maintaining intima to intima apposition. This stapling device is also inserted through a large incision in the host vessel wall and uses staples incorporated in the device to penetrate into tissue and secure the bypass graft to the host vessel.

Walsh, et al propose a similar end-side stapling device (U.S. Patents 4,657,019;
15 4,787,386; 4,917,087). This end-side device has a ring with tissue piercing pins. The bypass graft is everted over the ring; then, the pins penetrate the bypass graft thereby securing the bypass graft to the ring. The ring is inserted through a large incision created in the host vessel wall and the tissue piercing pins are used to puncture the host vessel wall. A clip is then used to prevent dislodgment of the ring relative to the host vessel.

20 The end-side stapling devices, previously described, require insertion through a large incision, which dictates that blood flow through the host vessel must be interrupted during the process. Even so, these and other clipping and stapling end-side anastomotic devices require significant time to create the anastomosis. Interruption of blood flow for a prolonged period of time increases the morbidity and mortality of grafting procedures, especially during aortic
25 aneurysm repair.

A need thus exists for fittings, grafts, and delivery systems capable of quickly producing an anastomosis between a graft and a host vessel or reattaching branching vessels

with minimal interruption of blood flow. These anastomoses must withstand the pressure exerted by the pumping heart and ensure blood does not leak from the anastomoses into the thoracic cavity, abdominal cavity, or other region exterior to the vessel wall. In addition, these anastomoses must prevent dislodgment even when the graft is subject to external forces or
5 motion of the aorta.

Summary of the Invention

The invention provides systems and components for improved treatment for aneurysms that extend to bifurcations and/or envelop branching vessels, especially aortic aneurysms. The
10 systems enable a physician to quickly and accurately position and secure a reinforcing graft. In addition, the invention provides processes to reattach branching vessels to a reinforcing graft positioned within and secured to a host vessel while minimizing the interruption of blood flow to the branching vessel during the procedure.

The invention provides extension grafts that are configured to lengthen a branching
15 vessel or other host vessel which may be too short to reach the desired anastomosis site. The extension grafts also provide a mechanism to expedite reattaching the branching vessel to the reinforcing graft or re-establish blood flow to a branching vessel without the need to cut the branching vessel. The invention includes reinforcing grafts that incorporate branches containing end-end fittings inserted into and secured to branching vessels without cutting the
20 branching vessels.

End-end fittings are provided securing reinforcing grafts or extension grafts to host vessels. Once positioned within the host vessel, the end-end fittings are secured to the host vessel by compressing the host vessel against the end-end fitting using retaining rings, strands of suture, or stitches placed around the host vessel at the end-end fitting interface.

25 The invention provides end-side fittings capable of securing branching vessels or extension grafts to the side of a reinforcing graft and/or host vessel. The end-side fitting embodiments can be configured to produce anastomoses between branching vessels and host

vessels such that only the endothelial layer of the branching vessel is exposed to blood flow. In addition, end-side fitting embodiments are provided that do not require a delivery system to insert the end-side fitting through the reinforcing graft wall and/or host vessel wall.

The delivery systems of the invention enable inserting an end-side fitting and branching
5 vessel combination or an extension graft through a host vessel wall, and in many cases also a reinforcing graft, without interrupting blood flow through the host vessel. In addition, the delivery systems of the invention enable inserting a reinforcing graft through a host vessel wall. One delivery system embodiment is a combination of a tear-away sheath, dilator, guidewire, and needle designed to be inserted into the host vessel at the desired anastomosis
10 site. The fitting and branching vessel combination is inserted through the tear-away sheath into the interior of the host vessel. After reattaching the branching vessel, the hub and valve of the tear-away sheath are split and the sheath is then separated and removed from around the branching vessel. A plunger is used to insert the branching vessel and fitting combination through the sheath and past the host vessel wall and graft wall. The plunger also protects the
15 branching vessel during insertion, especially when advancing past the hemostatic valve.

An alternative delivery system involves advancing a fitting embodiment directly through a puncture in the host vessel wall and graft without stopping or re-routing blood flow. The fitting is partially inserted through an incision and rotated past the host vessel wall and graft, into the interior of the host vessel. Optionally, a guidewire can serve as a passage to
20 rotate and advance the fitting past the host vessel wall and graft, and into the interior of the host vessel. Once inside the host vessel, the fitting is secured, thereby attaching the branching vessel to the host vessel.

Further features and advantages of the inventions will be elaborated in the detailed description and accompanying drawings.

25

Brief Description of Drawings

Figure 1 shows the anatomy of the aorta and branching vessels;

Figure 2 is a view of the abdominal aorta showing representative branching vessels with the iliac arteries and the abdominal aorta clamped;

Figure 3 is a partially sectioned view of the abdominal aorta with a reinforcing graft partially inserted into the vessel through an incision;

5 Figure 4 shows an insertion device for advancing the ends of a bifurcating graft into branching vessels;

Figure 5 shows a reinforcing graft inserted into the abdominal aorta and a vent enabling blood flow to branching vessels external to the reinforcing graft;

10 Figures 6a and b are end and side-sectional views of the vent positioned adjacent an end-end fitting of a reinforcing graft to permit blood flow external to the reinforcing graft;

Figure 7 is a side view of the abdominal aorta with the legs of the bifurcation secured to the iliac arteries and an incision through the vessel wall clamped;

15 Figure 8 is a partially sectioned view of a branching vessel secured to a reinforcing graft, also showing a delivery system accessing the interior of the reinforcing graft for deploying a branching vessel and fitting combination or an extension graft;

Figure 9 shows a secured reinforcing graft isolating an aneurysm with branching vessels secured to the reinforcing graft;

Figures 10a to c show an end-end fitting for securing tubular structures such as vessels and grafts to fittings using sutures;

20 Figures 11a and b show retaining rings used to bond tubular structures to fittings and host vessels in accordance with the invention;

Figure 12 shows an expanding tool used to expand and position a retaining ring;

Figures 13a to c show an end-end fitting for securing tubular structures to fittings;

Figures 14a to c show a delivery system provided in accordance with the invention;

25 Figures 15a to c are side, end, and cross-sectional views of a plunger;

Figure 16 shows a dilating sheath;

Figures 17a to f show an alternative sheath embodiment of the delivery system;

Figure 18 shows an end-side fitting using a latching mechanism to secure a tubular structure to a host vessel wall;

Figures 19a and b show an end-side fitting designed to compress the host vessel wall between two fitting components;

5 Figures 20a and b show an alternative end-side fitting secured to a host vessel wall;

Figures 21a to e show an end-side fitting deliverable past a host vessel wall without the need for a sheath;

Figures 22a and b show further alternative end-side fittings;

10 Figures 23a and b show a compression tool designed to atraumatically advance a compression ring over an end-side fitting;

Figures 23c and d show the compression tool in the activated position;

Figures 24a to c show an everting tool;

Figure 25 shows a bypass graft and fitting combination attached to a host vessel wall and incorporating a strain relief around the fitting;

15 Figure 26 shows a pin used to axially advance a retaining ring against an end-end fitting;

Figure 27 shows a holder used to support the end-end fitting while advancing the retaining ring using the pin shown in Figure 26;

20 Figures 28a to c show the securing of a tubular structure to an end-end fitting with a retaining ring by using the pin and holder shown in Figures 26 and 27, respectively;

Figure 29 shows a reinforcing graft having integrated extension grafts;

Figures 30a and b show a clamp and for temporarily closing incisions through a vessel wall; and

25 Figures 31a to f show an alternative insertion device for advancing and retracting the fitting through vasculature;

Detailed Description of the Preferred Embodiments

The embodiments of the present invention are intended to rapidly produce anastomoses between reinforcing grafts (or replacement grafts) and host vessels to treat vascular abnormalities such as aneurysms, fistulas, or other surgical indications requiring a reinforcing graft. The embodiments of the invention also provide devices to secure branching vessels to a reinforcing graft during surgical procedures in which the branching vessels would otherwise be occluded from blood flow (e.g. reattaching the renal arteries, mesenteric artery, celiac artery, and intercostal arteries during abdominal aortic aneurysm repair). The systems of the invention specifically address the management of abdominal aortic aneurysms, thoracic aortic aneurysms, and thoracoabdominal aortic aneurysms by mitigating risks of current surgical and percutaneous treatment modalities. In addition, the systems are useful in aortic root replacement procedures, extracranial carotid aneurysm repair, and other aneurysm treatments in which a reinforcing graft (or replacement graft) is secured to the host vessel and/or branching vessels are reattached to the host vessel.

The reinforcing grafts, replacement grafts, or extension grafts may be manufactured by extruding, injection molding, weaving, braiding, or dipping polymers such as PTFE, expanded PTFE, urethane, polyamide, polyimide, nylon, silicone, polyethylene, collagen, polyester (Dacron), composites of these representative materials, or other suitable graft material. These materials may be fabricated using one or a combination of the stated manufacturing processes. The graft may be coated, deposited, or impregnated with materials, such as paralyne, heparin solutions, hydrophilic solutions, or other substances designed to reduce thrombus formation. Reinforcing or replacement grafts may alternatively be a harvested vessel such as the saphenous vein.

Fittings

The fittings in accordance with the invention are designed to attach reinforcing grafts (or replacement grafts) to host vessels, attach extension grafts to host vessels, or reattach

branching vessels to reinforcing grafts or host vessels. The fittings are constructed from a metal (e.g. titanium), alloy (e.g. stainless steel or nickel titanium), thermoplastic, thermoset plastic, silicone or combination of the aforementioned materials into a composite structure; other materials may alternatively be used. The fittings may be coated with materials such as paralyne or other hydrophilic substrates that are biologically inert and reduce the surface friction. Alternatively, the fittings may be coated with heparin or thrombolytic substances designed to prevent thrombosis around the attachment point to the host vessel. The fittings consist of one or more components designed to secure a reinforcing graft to a host vessel, secure an extension graft to a reinforcing graft, attach an extension graft to a host vessel, or attach the ends of branching vessels to a reinforcing graft.

The fittings may be laminated between layers of graft material during fabrication of a synthetic graft, or may be secured to the reinforcing graft, the branching vessel, or the extension graft using a compression mechanism. Figure 28c shows a reinforcing graft or an extension graft 16 having one end secured to an end-end fitting 20 by compressing the graft material between at least two components (e.g. the end-end fitting 20 and a retaining ring). These components may lock together as a result of the interference fit between the components with the graft material compressed between the components or may incorporate a separate locking mechanism.

Figures 28a to c show the process of compressing a graft or other tubular structure 16 between an end-end fitting 20 and a retaining ring 22. As seen in Figure 28b, graft 16 is inserted through the inner surface of end-end fitting 20 and is advanced over the outer surface of retaining ring 22. This enables everting the graft 16 over fitting 20. The graft also can be advanced over the outer surface of the end-end fitting and through the inner surface of the retaining ring (not shown). Alternatively, the graft may be advanced over the outer surface of the end-end fitting and the retaining ring may be advanced over the side of the end-end fitting (not shown). A pin 24, shown in Figure 26, is advanced through the interior of the tubular structure from the end the retaining ring is to be advanced toward the end-end fitting. The pin

accommodates various diameter rings. The ridges 26 of the pin are used to push the ring over the fitting and graft interface. An inner channel may be incorporated into the pin. The inner channel allows the edge of the fitting and reinforcing graft combination to slide past the ridges so the ring can be placed a further distance onto the fitting and tubular structure interface. A holder 28, shown in Figure 27, is placed over graft 16 abutting the fitting. The holder also accommodates various diameter grafts and fittings. The pin is axially movable relative to the holder to permit advancing retaining ring 22 toward the end-end fitting 20. The retaining ring shown in Figures 28a to c extends to less than a complete circle to permit expansion over the end-end fitting as the retaining ring is advanced. As seen in Figure 28c, the graft is everted as the retaining ring is advanced, using the pin and holder, over fitting 20. The end-end fitting includes a notch in which the retaining ring fits to prevent axial dislodgment of the retaining ring once positioned. The holder and pin may also be used to compress two fitting components that lock axially and do not need to overlap. This does not require everting the reinforcing graft over the end-end fitting.

Using a ring or other compression mechanism to attach the fitting (end-end or end-side) facilitates securing the fitting anywhere along the graft or branching vessel. The primary benefit of being able to selectively secure the fitting to the reinforcing graft, the branching vessel, or the extension graft is the ability to specify the desired length of the graft or vessel and attach the end-end fitting to that established parameter. This gives flexibility to determine the extent of the aneurysm before tailoring the reinforcing graft to support the affected vasculature, assess whether the branching vessel and fitting combination will sufficiently reach the host vessel, or evaluate the length of extension graft needed to extend from the end of the branching vessel to the host vessel. In addition, this enables using biological grafts obtained by harvesting vessels, instead of synthetic graft materials.

An alternative method to tailor the length of the reinforcing graft or the extension graft, depending on physiologic differences, is to include end-end fittings at spaced apart intervals (e.g. 1 inch) along the graft. These spaced apart end-end fittings provide the operator with the

flexibility of shortening the graft to any length while still incorporating end-end fittings to facilitate securing the graft to the host vessel. In addition, the end-end fittings provide radial support along the graft to maintain graft patency and facilitate puncturing the graft wall when accessing the interior of the reinforcing graft with the delivery system for inserting the

5 branching vessel and end-side combination or an extension graft. Finally the spaced apart end-end fittings provide structures that the operator may secure to the host vessel using retaining rings or suture, as will be described below, to better secure the graft to the host vessel throughout the length of the graft.

Instead of incorporating end-end fittings at spaced apart intervals along the reinforcing

10 graft, the reinforcing graft may incorporate support members that accomplish the same goals as the numerous end-end fittings. The support members may be laminated between layers of graft material. The synthetic bypass graft encompassing support members may be fabricated by extruding, spraying, injection molding, or dipping a primary layer of graft material over a removable mandrel; positioning, winding or braiding the support members on the primary

15 layer; and extruding, spraying, injection molding, or dipping a secondary layer over the graft material/support member combination. The support members may be fabricated from a metal, alloy (e.g. stainless steel or nickel titanium), or polymer (e.g. nylon or polyester). Preferably, the support members have a shape memory. The support members may be manufactured with a wire material oriented in a serpentine pattern or a mesh defining a sufficiently large space

20 between wires. This configuration helps support the reinforcing graft and defines a space to puncture the reinforcing graft wall and access the interior of the reinforcing graft with the delivery system of the invention. The spacing of the wires, the diameter of the wires, and the annealing of the support members may be tailored to produce a spring characteristic that matches that of a compression mechanism used to compress the host vessel wall against the

25 end-end fittings (which in this case is the support members), also fabricated from a memory elastic material.

Figure 1 shows the anatomy of an aorta 30. The aortic root, not shown, runs into the thoracic aorta. The thoracic aorta runs around the aortic arch, bifurcates into the left subclavian artery, the branchiocephalic trunk, and the left common carotid artery, and extends into the abdominal aorta. The abdominal aorta bifurcates into the iliac arteries 32. Vessel bifurcations
5 are frequently enveloped by aortic aneurysms. As such, reinforcing or replacement grafts used to treat aortic aneurysms frequently support the affected bifurcations. For example, numerous reinforcing grafts used to treat abdominal aortic aneurysms include bifurcating legs that extend into the iliac arteries.

Branching vessels that extend away from the abdominal aorta include renal arteries 34,
10 celiac arteries, suprarenal artery, mesenteric arteries, phrenic arteries, and testicular arteries. Abdominal aortic aneurysms are frequently classified by their location relative to the renal arteries. As shown in Figure 1, infrarenal aneurysms (B-B) are located below the renal arteries; juxtarenal aneurysms (C-C) approach the renal arteries; pararenal aneurysms (D-D) include the renal arteries; and suprarenal aneurysms (E-E) extend above the renal arteries.
15 Thoracoabdominal aneurysms (F-F) are classified by type I, II, III or IV depending on their location relative to descending thoracic aorta and the abdominal aorta; most thoracoabdominal aneurysms envelop the renal arteries of the abdominal aorta.

The thoracic aorta extends from the abdominal aorta to the aortic root and defines bifurcations to the left subclavian artery, the branchiocephalic trunk, and the left common
20 carotid artery. Branching vessels that extend from the thoracic aorta include the aortic esophageal arteries, intercostal arteries, and bronchial arteries. The left main artery and right coronary artery branch off the aortic root.

Reinforcing Grafts

25 Reinforcing grafts may be fabricated from a sheet of graft material rolled into a tube with the sides bonded together, or a tube of graft material that defines a central lumen and contains at least two ends. For abdominal aortic aneurysms that require a bifurcated graft, the

reinforcing graft has three ends configured to match the bifurcation from the abdominal aorta to the left and right iliac arteries. For thoracic aortic aneurysms that require a bifurcated graft, the reinforcing graft has a geometry designed to match the curvature of the thoracic aorta with bifurcations capable of extending into the subclavian artery, left common carotid artery, and
5 branchiocephalic trunk. Other applications involving saccular or fusiform aneurysms located at vessel bifurcations also require bifurcated reinforcing grafts. Reinforcing grafts are designed to be inserted into a host vessel and extend along the interior surface of the host vessel. Once positioned and secured, the reinforcing graft isolates the host vessel wall and anything attached to the host vessel wall between the end-end fittings of the reinforcing graft from blood flow.

10 The reinforcing graft 18, as shown in Figure 29, may additionally include branches 36. Each branch 36 incorporates an end-end fitting 20 attached at the end of the branch. The end-end fittings may be laminated between layers of graft material or may be compressed between fitting components as described above. The branches facilitate attaching branching vessels to the reinforcing graft without the need for end-side fittings or extension grafts, described herein.
15 One method of securing branches 36 to the branching vessels is to insert the branches into the lumens of the branching vessels while positioning the reinforcing graft. Insertion devices described herein are used to position the branches. In addition, the positions of the orifices of the branches do not need to exactly match the orifices of the branching vessels. Instead, the branches may run between the reinforcing graft and the host vessel wall for a length before
20 they extend into the lumen of the branching vessels. This accommodates the varying anatomy between patients. Once positioned, end-end fittings 20 of branches 36 are secured to the branching vessels by producing end-end anastomoses.

The reinforcing graft may be directly inserted through an incision in the host vessel wall or through a delivery system described below. Alternatively, the reinforcing graft may be
25 inserted percutaneously using a catheter-based delivery system. The catheter-based delivery system incorporates modifications to the delivery system described below, which include

longer access and guiding devices to account for remote, percutaneous vessel access, as opposed to direct vessel access.

An insertion device 38 (Figure 4) is used to position the ends of the reinforcing graft (and branches, if present) at the desired host vessel location. The insertion device exerts force
5 against end-end fittings, already attached to the ends of the reinforcing grafts, to advance and retract the end-end fittings of the reinforcing graft within the vasculature. Insertion device 38 has two sections 39 that rotate about a pivot 40 to accommodate various reinforcing graft geometries and enable inserting the bifurcations of the reinforcing graft into the iliacs.

Another insertion device is a plunger 42 shown in Figure 15a and described below,
10 suited for inserting grafts attached to fittings through a delivery system and positioning the end-end fittings of the reinforcing graft, extension grafts, or branches at the desired host vessel location. For bifurcated reinforcing grafts and grafts containing branches, the insertion device individually positions the legs of the reinforcing graft or branches in the appropriate host vessel. The ends of the reinforcing graft, extension graft, and branches contain end-end fittings
15 such that, once positioned, the end-end fitting may be secured to the host vessel by producing end-end anastomoses described below.

Figures 31a to f show alternative insertion devices for positioning end-end fittings within the host vessel. Figures 31a and b show an insertion device 44 with a slide 46 rotated into a closed position. The insertion device is closed after placing the reinforcing graft and the
20 end-end fitting within a lumen defined by closed slide 46 and between the grasping members of 48 and the pushing member 50 of the insertion device. The pushing member 50 is attached to a handle 52 for remote handling of insertion device 44. Slide 46 is also axially movable relative to pushing member 50. Figures 31a and b show slide 46 separated from the pushing member and Figures 31c and d show the slide and pushing member in a closed configuration.
25 The slide and pushing member are closed to grab the end-end fitting to provide improved manipulations. This insertion device is capable of advancing, torquing, and retracting the end-end fitting through the vasculature. Insertion device 44 is adapted to grab the entire width of

the end-end fitting or just the distal end of the end-end fitting. Once the end-end fitting is positioned, slide 46 is rotated to an open configuration as shown in Figures 31e and f to permit removing from the side of the reinforcing graft, branch, or extension graft. Alternatively, the slide device is not rotatable relative to the pushing member. However, the slide still is axially manipulated to grab the end-end fitting for manipulations through the vasculature. This embodiment does not require placing the insertion device around the periphery of the reinforcing graft, branches, or extension graft and permits grabbing a small section of the end-end fitting.

10 Extension Grafts

Extension grafts are designed to lengthen a branching vessel that is not long enough to reach the desired anastomosis site of the host vessel (whether or not reinforced with a graft). The extension graft contains an end-end fitting at one end capable of producing an end-end anastomosis to the branching vessel. The extension graft has, at its opposite end, either an end-side fitting or an end-end fitting, depending on the application. An end-side fitting permits attaching the extension graft to an opening, created with the delivery system, in the reinforcing graft wall and/or host vessel wall to re-establish blood flow to the branching vessel. An end-end fitting enables attaching the extension graft to the end of another extension graft or a branch incorporated in the reinforcing graft.

20 The extension graft may be inserted into the host vessel prior to attaching the branching vessel, thereby maintaining blood flow to the branching vessel while securing the extension graft to the host vessel. Then, the branching vessel may be tied off, cut, quickly advanced over the free end of the extension graft, and secured to the end-end fitting, as will be described below. This minimizes the ischemia time associated with interrupting blood flow while reattaching the branching vessel. Alternatively, the free end of the extension graft may be inserted into the intact branching vessel using the delivery system, as described below. Once inserted into the branching vessel, the end-end fitting may be secured to the branching vessel

using retaining rings or suture. The extension graft routes blood flow from the interior of the reinforcing graft or host vessel, and into the branching vessel.

Delivery Systems

5 The delivery system embodiments of the invention for positioning the branching vessels are designed to quickly access the interior of the deployed reinforcing graft through a small puncture in a wall 54 of a host vessel 56 and the reinforcing graft wall 16. As such, the delivery systems are designed to prevent excess blood loss when accessing the interior of the reinforcing graft and deploying the branching vessel and fitting combination, thereby
10 eliminating the need to stop or re-route blood flowing through the host vessel. This approach also improves the leak resistance around the fitting due to elastic compression of the vessel wall and the reinforcing graft wall around the fitting. Additionally, the delivery system enables deploying an extension graft through host vessel wall 54 and reinforcing graft wall 16.

 The delivery system must permit removal from around the branching vessel or the
15 extension graft after securing the transected end of the branching vessel or the extension graft to the host vessel. Figures 14a to c show representative steps to position a branching vessel and fitting combination through a host vessel wall and a reinforcing graft wall. These steps also demonstrate the process for deploying an extension graft through the host vessel wall and the reinforcing graft wall.

20 A puncture device 58 (e.g. needle) is preloaded through a dilator 60 that has been preloaded through a sheath 62. The needle, dilator, and sheath combination is then positioned at the target anastomosis site. As Figure 14a shows, the needle is used to puncture host vessel wall 54 and the reinforcing graft 16, and is advanced into the interior of the reinforcing graft. The needle may be designed with a tapered or stepped distal end to restrict movement of the
25 needle beyond the end of the dilator and prevent perforating the opposite side of the host vessel or unwanted anatomy. A guidewire (not shown) may be advanced through the needle to provide a path over which the dilator and sheath may be advanced. When using a guidewire,

the needle may be retracted to prevent unwanted perforations or abrasions to the host vessel or adjacent anatomy. The needle does not necessarily need to be preloaded through the dilator, permitting the use of a larger diameter guidewire that better matches the inner diameter of the dilator. The dilator is then advanced over the needle or guidewire, past the host vessel wall, past the reinforcing graft wall, and into the interior of the reinforcing graft. Subsequently, the needle (if not already retracted to insert the guidewire) may be removed or retracted inside the dilator. The dilator is tapered to provide a smooth transition when advancing the dilator through the host vessel wall and reinforcing graft wall. The host vessel wall and reinforcing graft wall inherently form seals around the dilator preventing excess blood leakage from the host vessel.

Sheath 62 has a radius or tapered distal end forming a smooth transition from the dilator to the body of the sheath around the dilator. Once the dilator is positioned within the interior of the reinforcing graft, the sheath is advanced over the dilator and into the interior of the reinforcing graft. At this point, the dilator may be removed. This technique of inserting a sheath into a vessel over a dilator and needle is commonly used by physicians when performing the Seldinger technique during catheterization procedures or inserting I.V. catheters into veins for withdrawal of blood or introduction of medicines. The sheath and dilator may be constructed from polyethylene, or other polymer that may be extruded or molded into a tube. The sheath and dilator may incorporate a braided layer laminated between two polymer layers to resist kinking and improve the column strength and torque response. A taper and radius may be formed in the distal end of the dilator and sheath by thermally forming the raw tubing into the desired shape. In addition, the sheath may incorporate a softer distal tip fabricated by thermally bonding a short section of lower durometer tubing to the sheath or tapering the thickness of the sheath tubing.

The hubs on the sheath and dilator may be fabricated from polycarbonate, polyethylene, PEEK, urethane or other material, which may be injection molded, adhesively bonded, ultrasonically welded, or thermally bonded to the tube. A hub 64 of the sheath contains at least

one and preferably two grooves, slits, or series of perforations 66 along the hub to enable the operator to split the hub when removing the sheath from around the branching vessel. The hub of the sheath houses a hemostatic valve 68 constructed of silicone, urethane, or other material having a low durometer and a large percent elongation characteristic. The valve may be coated
5 with a lubricant such as silicone to facilitate insertion of the fitting and branching vessel combination or extension graft through the sheath. The hemostatic valve prevents excess blood loss through the sheath when positioned inside the vessel. The valve also incorporates at least one groove, slit, or series of perforations to permit separation when tearing the sheath from around the bypass graft. A side port (not shown) may be included to aspirate and flush the
10 sheath. The hub may alternatively be a separate piece from the tear-away sheath such that it may be independently removed from around the branching vessel. This hub would include a luer fitting to enable securing onto a mating piece of the tear-away sheath, or other mechanism to permit removably attaching the hub to the tear-away sheath. This hub may incorporate at least one groove, slit, or series of perforations to enable splitting the hub to form an opening to
15 remove the hub from around the bypass graft. Alternatively, the hub may include a slot, which during use is closed to prevent fluid from leaking, but can be aligned to form an opening for removal from around the bypass graft.

The ability to split is essential to removing the sheath from around a branching vessel when the sheath is unable to slide past the opposite end of the branching vessel. As shown in
20 Figure 14c, the sheath 62 may also be fabricated with at least one groove 66, slit, or series of perforations formed along the tube and hub to provide a guide to tear-away the sheath along at least one side, after securing the branching vessel to the host vessel wall and reinforcing graft wall. Alternatively, the sheath may include a section of tubing material already split into at least two sections such that the sheath tubing tends to continue to split into two pieces as the
25 two sections are pulled apart. When incorporating supporting material into a tear-away sheath to improve column strength, this material should ensure the sheath may be split along the grooves, slits, or perforations formed in the sheath. This supporting material may be fabricated

into two braided sections, or other support member sections oriented on opposite sides of the sheath such that the grooves reside along the spaces between the braided sections.

Alternatively, the supporting material may be strands of wire (stainless steel, nylon, etc.) laminated between layers of sheath material and oriented axially along the longitudinal axis of the sheath.

The length of the sheath should be limited to that required to access the interior of the reinforcing graft while ensuring short sections of exposed branching vessels or extension grafts may be inserted past the distal end of the sheath, especially when the branching vessel has been secured at the opposite end. To make the sheath suitable for less invasive access, a long side arm extension to the sheath may be incorporated to support the sheath during manipulations. The side arm should define two separable sections that permit splitting and remotely tear the sheath into two sections to remove from around the branching vessel.

Figure 16 shows an adaptation of a delivery system that combines the tear-away sheath and the dilating member into one component. The dilating sheath 70 contains at least one groove, slit, or series of perforations 66 that enables splitting the dilating sheath for removal from around the branching vessel or extension graft. The dilating sheath also contains a tapered distal end 72 that is designed to follow a needle or guidewire through a puncture in vessel wall 54 and/or the reinforcing graft wall, and expand the puncture to facilitate inserting the main section of the dilating sheath. The dilating sheath has a central lumen (not shown) adapted to pass the bypass graft and fitting combination. A plunger 88 is used to advance the branching vessel and fitting combination past the tapered end 98 of the dilating sheath and into the interior of the reinforcing graft. As discussed for the tear-away sheath, the dilating sheath contains a hub and hemostatic valve that permit splitting along groove, slit, or series of perforations 66.

Tapered end 72 must prevent collapsing while inserting through and opening the puncture site, and enable expanding so the bypass graft and fitting combination may be advanced into the host vessel lumen. The tapered end may be fabricated by cutting the end of

the sheath tubing into three or more sections such that each section tapers distally, forming the sections such that they create a single tapered distal end (the sections may overlap partially), and covering the tapered distal end with a material having a low durometer and a large percent elongation (e.g. silicone and urethane). The sections are formed such that they exert radial
5 force to prevent collapsing while the dilating sheath is advanced through the puncture site. The covering provides a fluid tight coating around the tapered end that elongates as the sections are spread apart; this enables expanding the diameter of the tapered end while the bypass graft and fitting combination are inserted through the tapered end. An alternative fabrication process eliminates the need for the covering by bonding the overlapping sections with a temporary low
10 strength adhesive. The low strength adhesive holds the position of the tapered end sections and produces a fluid tight interface between the sections but permits separating the sections as the plunger advances the bypass graft and fitting combination through the positioned dilating sheath.

An adaptation to the delivery system addresses conditions where the reinforcing graft or
15 extension graft is inserted through a large incision through the host vessel wall or through the end of a transected host vessel. A modified "hockey stick" sheath 74, (Figures 17a to f), has a tapered distal end 76 and a partially enclosed body. This hockey stick sheath is advanced through the incision or the open host vessel end, and expands the vessel wall. This way the reinforcing graft, extension graft, or branching vessel and fitting combination may be advanced
20 through the hockey stick sheath lumen and into the host vessel without catching on the vessel wall. This is especially important when the fitting has an outer diameter larger than the inner diameter of the host vessel such that the host vessel must be expanded to insert the fitting. The hockey stick sheath may incorporate an extension perpendicular to the longitudinal axis that provides a handle to manipulate the hockey stick sheath. In addition, the hockey stick sheath
25 may incorporate at least one spring-loaded jaw to grab the host vessel wall after access has been obtained and permit manipulating the expanded host vessel by using the hockey stick sheath. This is especially useful when accessing the end of a transected vessel, which requires

significant manipulations while positioning the extension graft into the lumen of the host vessel.

Plunger 42 is designed to insert the branching vessel and fitting as an attached unit, therefore it includes a lumen to protect the branching vessel while inserting the fitting into the interior of the reinforcing graft. The plunger is also used to advance the extension graft through the sheath and into the interior of the reinforcing graft or the host vessel lumen. A plunger is essential when inserting branching vessels or extension grafts that do not have adequate column strength to be pushed through the hemostatic valve of the sheath. After using the plunger to advance the branching vessel and fitting combination into the interior of the reinforcing graft, the plunger is contained between ends of the attached branching vessel and must be removed. The plunger 42 shown in Figures 15a to c includes an axial slot through the entire length of the plunger. The slot enables pulling the plunger from the side of the branching vessel when removing the plunger and permits pressing the plunger over the side of the branching vessel when placing the plunger over the branching vessel. One end 76 of this plunger has a short length stepped down to form a smaller outer diameter that fits inside the inner diameter of the fitting and provides a stable anchor to insert and manipulate the fitting during delivery of the bypass graft and fitting combination into the vessel. The other end 78 the plunger has the inner diameter reamed out and notched for a short length to fit over the outer diameter of the branching vessel and fitting combination during manipulations. The notched region may alternatively extend a sufficient length such that the plunger covers the exterior of the fitting to protect the fitting during insertion through the sheath. This feature is especially important when inserting end-side fittings that require constraining the petals in a reduced diameter profile for advancing through the sheath. This feature also helps constrain foldable or compressible fittings into a reduced diameter for insertion through a sheath having a smaller inner diameter than the expanded outer diameter of the fittings. Since this plunger maintains its integrity upon removal from the branching vessel, it may be used to deploy multiple branching vessel and fitting combinations.

End-End Anastomoses

End-end fittings 20 may be incorporated in the reinforcing graft and the extension graft to facilitate securing the graft to a host vessel. The end-end fittings are configured to be
5 inserted into the lumen of the host vessel and contact the interior surface of the host vessel throughout the cross-section of the host vessel. A groove may be fabricated on the outer surface of the fitting to prevent axial movement of the retaining ring, after positioning the retaining ring over the host vessel to fitting interface. The retaining rings are designed to produce an interference fit between the reinforcing graft or the extension graft and the host
10 vessel to hold the graft in place and prevent leaking at the attachment point.

Figures 11a and b show embodiments for retaining ring 22 used to secure the end-end fitting 20 of the reinforcing graft or the extension graft to the host vessel. The retaining ring may have a rectangular, circular, semicircular, or elliptical cross-section. The retaining ring may include eyelets to facilitate positioning the retaining ring around the host vessel to fitting
15 interface and may be used to suture the retaining ring closed for additional support. The retaining ring may be fabricated from a metal, alloy, thermoplastic material, thermoset, or composite. However, the retaining ring must permit approximately 30% enlargement in diameter without becoming permanently deformed. Thus, after placement, the retaining ring will compress the host vessel against the fitting and form a secure seal. As a result, the
20 preferred material for the retaining ring is a memory elastic alloy such as nickel titanium exhibiting a stress-induced martensite characteristic or a spring steel such as 17-7.

The retaining ring 22 in Figure 11a is a preshaped member wound beyond a single turn. One representative fabrication process for the preshaped retaining ring involves forming the raw material into a desired geometry and exposing the material to sufficient heat to anneal the
25 material into this predetermined shape. This process applies to metals, alloys (e.g. nickel titanium), polymers, or composites of the aforementioned materials. The preshaped retaining ring configuration is expanded by inserting the expansion tool into the middle of the retaining

ring and opening the expansion tool thereby enlarging the diameter of the retaining ring. Once the retaining ring is positioned, the force causing the retaining ring to enlarge is removed causing the retaining ring to return towards its preformed shape thereby compressing the host vessel against the fitting.

5 The retaining rings do not necessarily need to incorporate elastic memory characteristics. For example, retaining ring 22 in Figure 11a may be manufactured from a deformable material and crimped over the tubular structure to fitting interface or host vessel wall to fitting interface for securing purposes. Figure 11b shows another retaining ring 22 that does not incorporate elastic memory characteristics. This retaining ring is opened for
10 positioning around the bypass graft to fitting interface or the host vessel to fitting interface and is closed, causing teeth 80 to engage and lock the retaining ring in the closed position. Further closing the retaining ring causes the diameter to decrease and exert additional compression force.

 A representative expansion tool 82 is shown in Figure 12. This expansion tool is
15 designed to expand the retaining ring by pulling the ends of the retaining ring relative to an anchor point. A stylet 84 holds the retaining ring in place and produces the anchor point. Legs 86 of the expansion tool have notches positioned at the edges of the retaining ring. The legs rotate about a pivot pin 88 fixed to the handle. When the knob 90 is advanced relative to the handle, the legs are configured to move radially outward thereby opening the diameter of the
20 retaining ring. Once positioned around the host vessel to fitting interface, tension on the knob is released allowing the retaining ring to compress the host vessel against the fitting.

 Figures 10a to b show methods of suturing a host vessel to an end-end fitting. The end-end fitting 20 has notches 92 designed to provide an indentation to secure a host vessel using the retaining ring as described above, or suture 94 as described below. Once the reinforcing
25 graft is advanced into the lumen of the host vessel, one or more strands of suture 94 are tied around the host vessel and located in the notches of the end-end fitting 20 thereby producing a fluid tight seal. Alternatively, stitches may be created at fixed intervals around the host vessel

wall to end-end fitting interface. The suture is fed through the host vessel wall from the external surface of the host vessel, pushed around the end-end fitting or through the end-end fitting when the fitting is fabricated from a compliant material, pulled back through the host vessel wall on the opposite end of the fitting, and tied into a knot. Needles attached to the strands of suture permit puncturing the vessel wall (and fitting for compliant fitting materials) and advancing the suture for forming the stitches. These methods permit suturing the reinforcing graft or extension graft to a host vessel while blood is flowing through the host vessel.

10 End-Side Anastomoses

An embodiment for producing an end-side anastomosis between a branching vessel or extension graft, and a reinforcing graft is shown in Figure 18. After the branching vessel and fitting combination or extension graft is inserted partially through the host vessel wall 54 and the reinforcing graft wall, a self-locking compression ring 96 is advanced over teeth incorporated in the fitting. A ratcheting mechanism 98 prevents the self-locking component from dislodging from the fitting. The distal end of compression ring 96 is designed to match the flared end of the fitting. Therefore, as the compression ring is further advanced relative to the fitting, the host vessel wall and the reinforcing graft wall become compressed between the compression ring and the flared end of the fitting producing a fluid tight, secure bond. This embodiment is capable of bonding the host vessel wall and the reinforcing graft wall to the branching vessel and fitting combination or the extension graft.

For applications where the operator wants to evert the end of a tubular structure (e.g. branching vessel) over the fitting, prior to deploying and securing the fitting to the host vessel wall, an everting tool 100 is used to wrap the tubular structure around the end of the fitting. One everting tool embodiment shown in Figures 24a to c may be inserted into the distal end of the tubular structure. The distal end 102 of the everting tool is designed to fit through the lumen of the tubular structure (e.g. branching vessel) 104 and the inner diameter of the fitting

20. Proximal to the everting tool distal end is a tapered or curved region 106 which causes the tubular structure to wrap around the distal end of the fitting as the tubular structure and fitting are advanced over the everting tool. A retaining ring 22 is housed around the everting tool and is advanced over the tubular structure and fitting to secure the tubular structure to the fitting.

5 An alternative embodiment for performing an end-side anastomosis is shown in Figures 19a and b. The embodiment shown in Figures 19a and b includes a fitting 20 with a tubular structure (e.g. branching vessel) 104 everted over the distal end of the fitting. A retaining housing 108 may be used as a compression mechanism to secure the branching vessel or extension graft to the fitting 20 for configurations when the retaining housing is expanded or
10 advanced over the fitting to compress the branching vessel or extension graft against the fitting in an everted orientation. One retaining housing permits radial expansion during placement over the branching vessel and fitting, yet has a preshaped memory to compress around the branching vessel and fitting thereby securing the branching vessel to the fitting. This retaining housing 108 has petals 110 at its distal end, which compress into a low profile during delivery
15 through a sheath and expand radially once deployed inside the host vessel wall and reinforcing graft wall.

 The number of petals incorporated in the retaining housing design depends on the size of the branching vessel. In this illustrated embodiment, eight petals are used. The petals 110 may be oriented at fixed intervals or at varying angles; the petals may also have a fixed length
20 or varying lengths depending on the requirements for insertion and engagement against the host vessel wall. After advancing the tubular structure (e.g. branching vessel or extension graft) and fitting through a sheath and past the host vessel wall and the reinforcing graft wall, the fitting is advanced beyond the end of the sheath and is no longer constrained by the sheath, thus expands towards its resting configuration. Then the tubular structure and fitting
25 combination is gently retracted to engage the reinforcing graft wall with the petals. For mechanical securing, a compression ring 112 is advanced over the fitting thereby compressing the host vessel wall and the reinforcing graft wall against the petals of the retaining housing.

To optimize the contact from the petals to the host vessel wall and the reinforcing graft wall, the petals may be oriented at an angle less than 90 degrees between the petals and the proximal portion of the fitting. Alternatively, the petals may be curved towards the proximal portion of the fitting. In addition, a stop may be incorporated in the fitting to prevent over-compressing the reinforcing graft wall and the host vessel wall against the petals using the compression ring. Such features better ensure that the distal ends of the petals maintain intimate contact to the host vessel wall and the reinforcing graft wall when the compression ring is secured to the fitting.

As shown in Figure 19a, the retaining housing 108 may incorporate a locking mechanism 114 with which to secure the compression ring. For example, compression ring 112 can incorporate a screw mechanism that matches threads in the retaining housing. To reliably screw a compression ring onto a retaining housing, this threaded retaining housing has a fixed diameter and is not expandable. The threads are oriented only along the sections of the retaining housing configured to engage the compression ring. The compression ring is alternatively locked in place using a ratchet mechanism, adhesives, sutures, or other attachment means to secure the compression ring in place. The compression ring for this embodiment incorporates two components: 1) a distal, flexible o-ring or disk 116 designed to produce a fluid tight seal and prevent damaging the vessel wall by excess compression; 2) a proximal, more rigid locking ring 118 used to maintain the position of the o-ring or disk relative to the host vessel wall and the reinforcing graft wall. The locking ring is designed to match the threads incorporated in the retaining housing.

Figures 20a and b show another fitting 20 used to produce an end-side anastomosis. In this embodiment, the fitting incorporates petals 110 that collapse into a low profile during delivery through a sheath and extend radially outward once deployed into the interior of the reinforcing graft. In this embodiment, the branching vessel or the extension graft is advanced over the outside of the fitting and is compressed against the fitting using a retaining ring 22.

For extension grafts, the fitting may alternatively be laminated between layers of graft material. A compression ring 112 is still advanced over the fitting, after deploying the fitting into the interior of the reinforcing graft, and is used to compress the host vessel wall and the reinforcing graft wall against the deployed petals of the fitting. This secures the fitting to the host vessel wall and the reinforcing graft wall. As discussed previously the fitting incorporates a locking mechanism 104 to prevent axial motion of compression ring 112.

All fittings that incorporate petals and compression rings used to produce end-side anastomoses may be configured to produce a selected angle between the fitting axis and the interior of the reinforcing graft. In addition, the proximal end of the fitting may incorporate slots extending radially around a portion of the fitting and at specified intervals along the fitting. The slots institute flexibility in the fitting to permit slight movement of the fitting but maintain radial stiffness to prevent kinking of the extension graft or the branching vessel.

Figures 23a to d show a compression tool 120 designed to advance a compression ring over an end-side fitting without dislodging the fitting, or damaging the fitting, the tubular structure, the reinforcing graft wall, or the host vessel during the securing process. Figures 23a and b show the compression tool in the relaxed position. The compression tool has a front handle piece 122 and a rear handle piece 124 spread apart in the relaxed position. The handle pieces are squeezed together (activated) to advance the compression ring over the end-side fitting as shown in Figures 23c and d. The compression tool may be spring loaded to return to the relaxed position when the force causing the handle pieces to squeeze together is removed. The compression tool has a slot 126 through the distal section adapted to fit over the side of the tubular structure and fitting. This eliminates the need to preload the tubular structure through the compression tool prior to the procedure, and facilitates removing the compression tool after securing the tubular structure. As shown in Figure 23b, the compression tool incorporates a slide 128 adapted to move along grasping legs 130. The grasping legs are anchored to the rear handle piece, and the slide is advanced by squeezing the front handle piece towards the rear handle piece. The slide and the grasping legs are configured to define slot 126 through the

distal section of the compression tool. The grasping legs are flared outward as they extend distally to fit around the proximal end of the fitting in the relaxed state and close around the fitting (shown in Figure 23d) as the slide is advanced over the grasping legs. Slide extensions 132 are either incorporated in the distal end of the slide design or are bonded to the slide, depending on the manufacturing process and whether the slide extensions are fabricated from the same material as the slide. The slide extensions exert a radial spring force to close the grasping legs around the fitting, and push the compression ring over the end-side fitting. The compression ring is placed over the grasping legs and against the slide extensions prior to advancing the compression ring over the fitting. Then, the compression tool is positioned so the grasping legs extend over the proximal end of the end-side fitting. The front handle piece is squeezed toward the rear handle piece causing the slide to advance over the grasping legs. Simultaneously, the grasping legs close around the fitting temporarily securing the compression tool to the fitting, and the compression ring is advanced over the fitting. This compression tool provides an anchor for grabbing the proximal end of the fitting and advancing the compression ring. This facilitates compressing the host vessel wall and the reinforcing graft wall against the petals of the fitting.

Figures 21a to e show a fitting 134 for producing an end-side anastomosis that compresses the vessel wall between two fitting components. In this embodiment, the fitting incorporates a flared distal region 136 having a slot 138 that defines two edges. The slotted distal end of the fitting is inserted through a puncture of the vessel wall and the reinforcing graft wall by positioning the edge of the slotted fitting at the puncture site, angling the distal flared region so the edge may be further advanced through the host vessel wall and the reinforcing graft wall, and rotating the fitting. Upon further rotation of the fitting, the entire flared region of the fitting is advanced into the interior of the reinforcing graft, as shown in Figure 21d. Then a compression ring 112 is positioned over the fitting and past a locking mechanism 140 (e.g. tabs) thereby compressing the host vessel wall and the reinforcing graft wall between the flared distal end and the compression ring, as shown in Figure 21e.

An alternative screw-in fitting 141 is shown in Figures 22a and b. In this configuration, a guidewire is inserted through the host vessel wall and the reinforcing graft wall, into the interior of the reinforcing graft by puncturing the host vessel wall and the reinforcing graft wall with a needle and inserting the guidewire through the lumen of the needle. The needle is removed from around the guidewire after inserting the guidewire through the host vessel wall and the reinforcing graft wall. An insertion tubing 142 containing a central lumen follows the periphery of flared end and is adapted to pass a guidewire. The guidewire is fed through insertion tubing 142 to facilitate screwing the fitting past the host vessel wall and the reinforcing graft wall. The insertion tubing of the fitting extends approximately 40% to 80% around the flared end circumference. Alternatively, the insertion tubing may be configured in sections extending around the circumference of the flared end so the physician may determine how far around the flared end the guidewire must extend to rotate the flared end past the host vessel wall and the reinforcing graft wall. A slot 138 through distal flared end 136 is adapted to accept the thickness of the host vessel wall and the reinforcing graft wall and enables screwing the fitting through the host vessel wall and the reinforcing graft wall. As the screw-in fitting is advanced over the guidewire and rotated, the fitting simultaneously expands the puncture through host vessel wall and the reinforcing graft wall, and inserts more of the distal flared end into the interior of the reinforcing graft. Once the flared end of the fitting is inserted into the reinforcing graft interior, the guidewire is removed and the fitting is secured using a compression ring as described above, applying adhesives to the bond, suturing the fitting, or other bonding process.

Additional Fitting Features

Additional features may be included in any of the fitting configurations described above. Figure 25 shows a fitting 144 similar to the disclosed configurations having a strain relief 146 just proximal to the anastomosis. This strain relief provides additional support to the tubular structure (e.g. branching vessels) while preventing kinking. In addition, the strain relief

reduces the profile of the fitting, making it less traumatic during use. The strain relief may be substituted by making the proximal end of the end-side fitting flexible. Radial slots may be fabricated in the proximal end of the fitting to maintain radial stiffness but increase axial flexibility to function as a strain relief capable of preventing kinking of the tubular structure 64 relative to the host vessel wall.

Another important feature is the incorporation of holes, notches, and slots in the fitting, fabricated by laser drilling, EDM, milling, or other manufacturing process. The fitting may alternatively be covered with a porous material, such as collagen, fibrinogen, gelatin, and urethane, to define a surface characterized by holes, notches, and slots. The incorporation of holes, notches and slots in the fitting provide a surface to encourage neointimal cell growth. This is especially important for fitting surfaces exposed to blood flow.

Aortic Aneurysm Treatment

A process for securing a reinforcing graft to the aorta and reattaching branching vessels directly applies to treatment of abdominal aortic aneurysms, thoracic aortic aneurysms, and thoracoabdominal aortic aneurysms. In addition, this process addresses aortic root replacements and subsequent reattaching of the left main artery and right coronary artery to the replacement graft. However, the process for securing a reinforcing graft and reattaching the branching vessels will be described specifically for the treatment of abdominal aortic aneurysms:

1. Clamp the abdominal aorta 30 proximal and distal to the aneurysm using vessel clamps 148, as shown in Figure 2. If the aneurysm extends to the bifurcations clamp the iliac arteries 32 instead of the distal region of the abdominal aorta.
2. Cut an incision 148 through abdominal aorta 30 long enough to insert a reinforcing graft 16 or 18.
3. Insert the reinforcing graft through the incision and position the end-end fittings 20 of the reinforcing graft such that the reinforcing graft envelops the aneurysm, as

shown in Figure 3. An insertion tool 38 such as that shown in Figure 4 is used to position the end-end fittings 20 at the desired host vessel locations.

4. Secure the distal end-end fitting 20 of the reinforcing graft to the abdominal aorta using a compression mechanism 22 (e.g. retaining ring), as shown in Figure 5.

5 Bifurcating reinforcing grafts contain two distal end-end fittings 20 that are to be secured using compression mechanisms 22 (e.g. retaining rings) to the common iliac arteries 32.

5. Remove vessel clamps 148 to re-establish blood flow through the reinforcing graft 18 to the peripheral vasculature and through the space 150 between the external surface of the reinforcing graft 18 and the abdominal aorta vessel wall 54, as shown in Figure 5. Blood flowing through the space 150 perfuses the intact branching vessels 152.

6. Insert a vent 154 between the end-end fitting 20 of the proximal end of the reinforcing graft 18 and the abdominal aorta 56, as shown in Figures 5, 6a, and 6b. The vent includes an opening at the distal end and holes 156 along the side that enable blood flow to pass into the space 150 between the reinforcing graft and the abdominal aorta vessel wall. A temporary compression mechanism that resembles a retaining ring 22 may be used to hold the proximal end-end fitting and the vent in place.

7. Clamp the incision 149 closed such that vent 154 is held in place, as shown in Figure 7. An incision clamp 158 such as that shown in Figures 30a and b may be used to temporarily close the incision. The incision clamp has mating legs 160 that rotate relative to a pivot 162 that is spring loaded so the resting configuration of the incision clamp is closed. Two handles 164 are squeezed to rotate the legs and open the incision clamp for positioning along the sides of the incision. Once positioned, the handles are released thereby closing the incision. For subsequent removal, the handles are once again squeezed opening the legs.

8. Near each branching vessel 152, puncture the abdominal aorta vessel wall and the reinforcing graft wall using the delivery system, as shown in Figure 8. To better puncture the reinforcing graft wall, the puncture device of the delivery system may be oriented at an acute angle relative to the axis of the reinforcing graft and advanced along the lumen of the reinforcing graft. This prevents the reinforcing graft from radially collapsing which may cause the puncture device to perforate through the opposite side of the reinforcing graft wall and the abdominal aorta vessel wall. Alternatively, a mechanical supporting device may be inserted through the femoral artery (or other peripheral vessel) and into the abdominal aorta, and be positioned to exert radial force against the reinforcing graft wall at the puncture site (not shown). Such a mechanical expansion device is described in pending U.S. patent application "Mechanical Stent and Graft Delivery System" Serial No. 08/911,838, filed August 15, 1997, incorporated in its entirety herein by reference. This mechanical expansion device may be used to support the reinforcing graft wall, permit blood to flow through the expansion strands, and provide a space between strands so the mechanical device does not obstruct puncturing through the reinforcing graft wall. The reinforcing graft may alternatively incorporate support structures at spaced intervals to maintain graft flexibility yet provide radial support for puncturing through the reinforcing graft, as will be described later.
9. Dilate the puncture site and position the delivery sheath 62 through the abdominal aorta vessel wall 22 and the reinforcing graft wall 24.
10. Tie off or clamp the branching vessel. Cut the branching vessel 152 and attach it to an end-side fitting 20, as shown in Figure 8.
11. Advance the branching vessel and fitting combination through the delivery sheath 62, as shown in Figure 8.
12. Secure the end-side fitting 20 to the reinforcing graft wall and the abdominal aorta vessel wall using a compression ring.

13. Steps 10 – 12 may be modified by using an extension graft attached to the side of the reinforcing graft wall and the abdominal aorta vessel wall using an end-side fitting 20, as shown in Figure 8. The extension graft is secured prior to cutting the branching vessel and attaching the branching vessel to the end-end fitting 20 of the extension graft. The end-end fitting 20 of the extension graft may alternatively be inserted into the branching vessel using a delivery system, and secured with a compression mechanism (e.g. retaining ring) without having to cut the branching vessel. With this process, the extension graft is secured to the reinforcing graft wall and abdominal aorta vessel wall prior to inserting and securing the extension graft to the branching vessel. Therefore blood continuously flows through the branching vessel before, during, and immediately after securing the extension graft to the branching vessel.
14. Execute steps 8 – 13 for all remaining branching vessels. Bifurcating extension grafts 166 may be used to attach more than one branching vessel to the reinforcing graft wall and abdominal aortic aneurysm vessel wall using a single end-side fitting 20, as shown in Figure 9. Each of the bifurcations of this extension graft 166 includes end-end fittings 20 against which the branching vessels may be compressed using a compression mechanisms 22 (e.g. retaining rings).
15. Remove the vent from the incision, as shown in Figure 9.
16. Secure the proximal end-end fitting 20 of the reinforcing graft to the abdominal aorta using a compression mechanism 22 (e.g. retaining ring or suture), as shown in Figure 9.
17. Remove the incision clamp 158 and inspect the space 150 between the reinforcing graft and the abdominal aorta for leaks. Adjust the end-end fittings 20 of the reinforcing graft 18 to correct for any detected leaks.
18. Stitch 168 the incision closed.

The process described above may be modified to account for reinforcing grafts that may be compressed into a reduced diameter, inserted into the abdominal aorta, and positioned at the desired locations using a delivery system as opposed to requiring an incision. For this situation, blood flow through the host vessel would not need to be stopped at anytime during the procedure. Steps 1 – 3 would be substituted with the following: 1) Insert a delivery sheath into the interior of the host vessel; 2) Advance the reinforcing graft, compressed into a reduced diameter for insertion through the sheath, into the host vessel; 3) Position the end-end fittings at the desired host vessel locations using a steerable or preshaped insertion device. The vent tube, if necessary, would be inserted through the delivery sheath. After securing the reinforcing graft and reattaching the branching vessels, the vent tube would then be removed. After securing the proximal end-end fitting of the reinforcing graft, the opening defined by the delivery sheath would be stitched closed.

The delivery systems are capable of directly accessing the abdominal aorta, or percutaneously accessing the abdominal aorta from the femoral artery, popliteal artery, or the iliac artery. With direct access to the abdominal aorta, the delivery sheath may have a substantially larger diameter. This decreases the extent at which the end-end fittings of the reinforcing graft must be compressed into a reduced diameter. Therefore, end-end fittings capable of exerting substantial radial force may be used to adequately counteract the compression force exerted by the compression mechanism (retaining rings) when securing the host vessel wall between the end-end fitting and the compression mechanism. In addition, larger delivery systems facilitate positioning of the end-end fitting using an insertion tool because of the insertion tool has greater freedom of movement.

The process for positioning a reinforcing graft and re-establishing blood flow to branching vessels may modified for situations where the reinforcing graft includes branches which terminate into end-end fittings, as shown in Figure 29. Branches would be inserted into the branching vessels while positioning the reinforcing graft inside the abdominal aorta. As specified previously, this may be performed through an incision or through a

delivery system. Insertion devices, described below, are used to position the branches. When inserting the ends of the reinforcing graft and the branches through a delivery system, the insertion device preferably incorporates a steering mechanism to remotely manipulate the end-end fitting to the appropriate vessel location. The orifices of the branches do not need to be located exactly at the orifices of the branching vessels. Instead, branches 36 run between the reinforcing graft and the host vessel wall for a length before the branches extend into the lumen of the branching vessels; this accommodates the varying anatomy between patients. To ensure patency of the branches especially where the branches are bent such that they extend parallel to the reinforcing graft for a length, the branches may incorporate a support structure, such as a helix or mesh of a metal alloy wire (e.g. nickel titanium). Once positioned inside the branching vessels, the end-end fittings 20 of the branches are secured to the branching vessels by producing end-end anastomoses, as described below.

An alternative process for positioning and securing reinforcing grafts having branches 36 is to position the reinforcing graft into the abdominal aorta, as previously discussed, and fish the branches through the host vessel wall. Once the distal end-end fitting of the reinforcing graft is secured and the proximal end is positioned, the branches 36 may be fished through the abdominal aorta wall. To fish a branch 136 through a host vessel wall, a small incision is created near the end-end fitting of the branch and a clamp is inserted through the incision to grab the end-end fitting and pull the branch through the host vessel wall. The location of the end-end fitting is determined from outside the host vessel wall by feeling for the more rigid end-end fitting. An alternative method to fishing a branch 36 through the host vessel wall is to insert a wire having a hook through a small puncture in the host vessel wall and grab the branch with the inside surface of the wire-hook to pull the branch outside the host vessel wall. To prevent excess blood loss, the branches may be tied off until being fished through the host vessel wall, at which time the ties may be removed. The branches incorporate end-end fittings to permit advancing the branching vessels, once cut, over the end-end fittings and securing with a compression mechanism (e.g. retaining ring or suture). Alternatively, the

end-end fittings of the branches may be compressed into a reduced diameter for insertion into the intact branching vessels through a delivery system of the invention and secured to the branching vessels using compression mechanisms (e.g. retaining rings or suture).

The processes described above are for abdominal aortic aneurysms. However, the processes also apply to securing a reinforcing graft to the aorta and reattaching branching vessels for the treatment of thoracic aortic aneurysms, and thoracoabdominal aortic aneurysms. In addition, the processes apply aortic root replacements and subsequent reattaching of the left main artery and right coronary artery to the replacement graft.

10 Other Aneurysm Treatments

With slight modifications to the embodiments and processes described above, accounting for varying vessel diameters, other aneurysms may be treated. For example, extracranial carotid aneurysms requiring interposition grafts to reattach the internal carotid artery and the external carotid artery to the common carotid artery after removing the aneurysm may be treated with the embodiments and processes of the invention. An interposition graft consisting of a length of saphenous vein or synthetic graft may be configured to contain end-end fittings to facilitate attaching the interposition graft between the common carotid artery and either the internal or external carotid artery. As previously described, the interposition graft may be inserted through an incision in the host vessel wall or a delivery system accessing the interior of the host vessel through a puncture. Alternatively, the host vessels may be transected to remove the aneurysm tissue and attached to the end-end fittings of the interposition graft. The remaining one of the internal or external carotid artery is then attached to an end-side fitting, with or without an extension graft, to facilitate securing it to the interposition graft. The process and devices described herein for reattaching branching vessels are used to secure the remaining host vessel to the interposition graft. Alternatively, especially when using synthetic graft materials, the interposition graft may be fabricated with a bifurcation to facilitate attaching the common carotid artery to the internal carotid artery and the external carotid

artery. The ends of the bifurcated interposition graft contain end-end fittings to facilitate attaching the host vessels.

The embodiments and processes of the invention may also be used to treat other types of aneurysms such as cerebral aneurysms, peripheral aneurysms including femoral and
5 popliteal artery aneurysms, renal artery aneurysms, splanchnic artery aneurysms, hepatic artery aneurysms, celiac artery aneurysms, gastric and gastroepiploic artery aneurysms, pancreatic and pancreatoduodenal artery aneurysms, jejunal aneurysms, ileal and colic artery aneurysms, and mesenteric artery aneurysms, whether or not the treatment regimen requires reattaching branching vessels.

10 When treating aneurysms that do not require reattaching branching vessels, using the embodiments and processes of the invention, the reinforcing graft may be inserted through the host vessel wall using an incision or a delivery system of the invention. Once the end-end fittings of the reinforcing graft are positioned within the host vessel such that the graft envelops the aneurysm, the end-end fittings are secured with compression mechanisms (e.g. retaining
15 rings) as described.

When aneurysms envelop branching vessels that feed organs susceptible to ischemic time, perfusion through the branching vessels and host vessel may be maintained while deploying the reinforcing graft, and reattaching branching vessels, as described for abdominal aortic aneurysm treatment above. Briefly, the reinforcing graft may be inserted through an
20 incision, which requires temporarily interrupting blood flow through the host vessel while positioning the end-end fittings. Alternatively, the reinforcing graft may be inserted through a delivery sheath, as described herein, which does not require stopping blood flow through the host vessel while deploying the reinforcing graft through the host vessel wall and positioning the end-end fittings. The distal end-end fitting(s) of the reinforcing graft are then secured to
25 the host vessel using compression mechanisms (e.g. retaining rings), as described. Blood is permitted to perfuse through the space between the proximal end-end fitting and the host vessel wall to the branching vessels enveloped by the reinforcing graft. A delivery sheath is then

deployed through the host vessel wall and reinforcing graft and the branching vessel is tied at the orifice, cut, attached to an end-side fitting, deployed through the delivery sheath, and secured to the reinforcing graft and host vessel using a compression ring. As described for abdominal aortic aneurysm treatment, extension grafts may be used to lengthen the branching vessel (especially when part of the branching vessel was diseased and needed to be removed), enable reattaching the branching vessel without having to cut the branching vessel, or expedite reattaching the branching vessel. After all branching vessels have been reattached, the proximal end-end fitting of the reinforcing graft is secured to the host vessel using a compression mechanism (e.g. retaining ring). Any incisions or punctures through the vessel wall would then be stitched closed.

What is Claimed is:

1. A system for treating aneurysms including:

A reinforcing graft adapted to be inserted into a vessel and positioned between at least

5 two vessel locations to isolate an aneurysm from blood flow;

Two feedings attached to respective first and second ends of the reinforcing graft; and

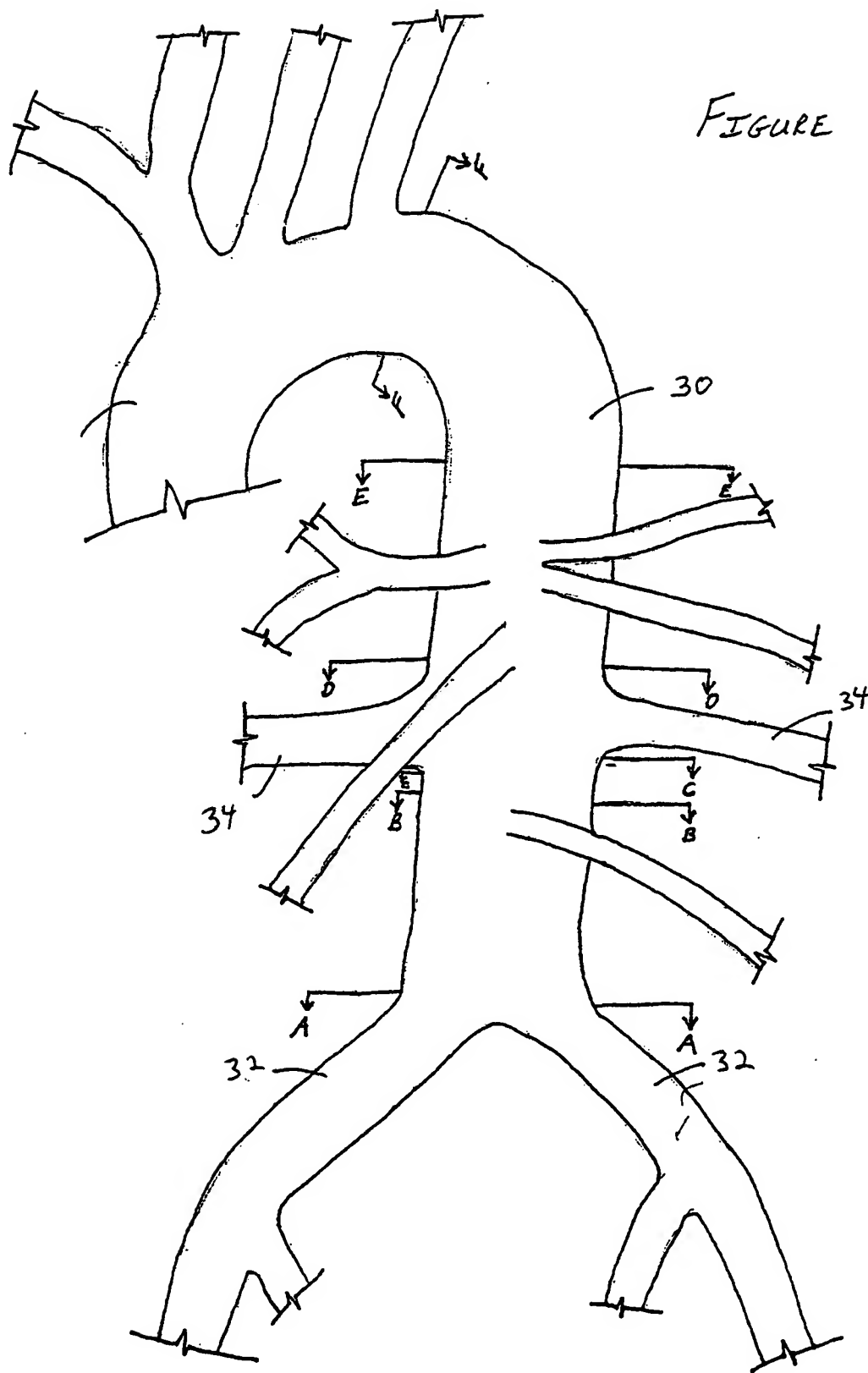
Two compression mechanisms adapted to fit at least partially around the vessel and

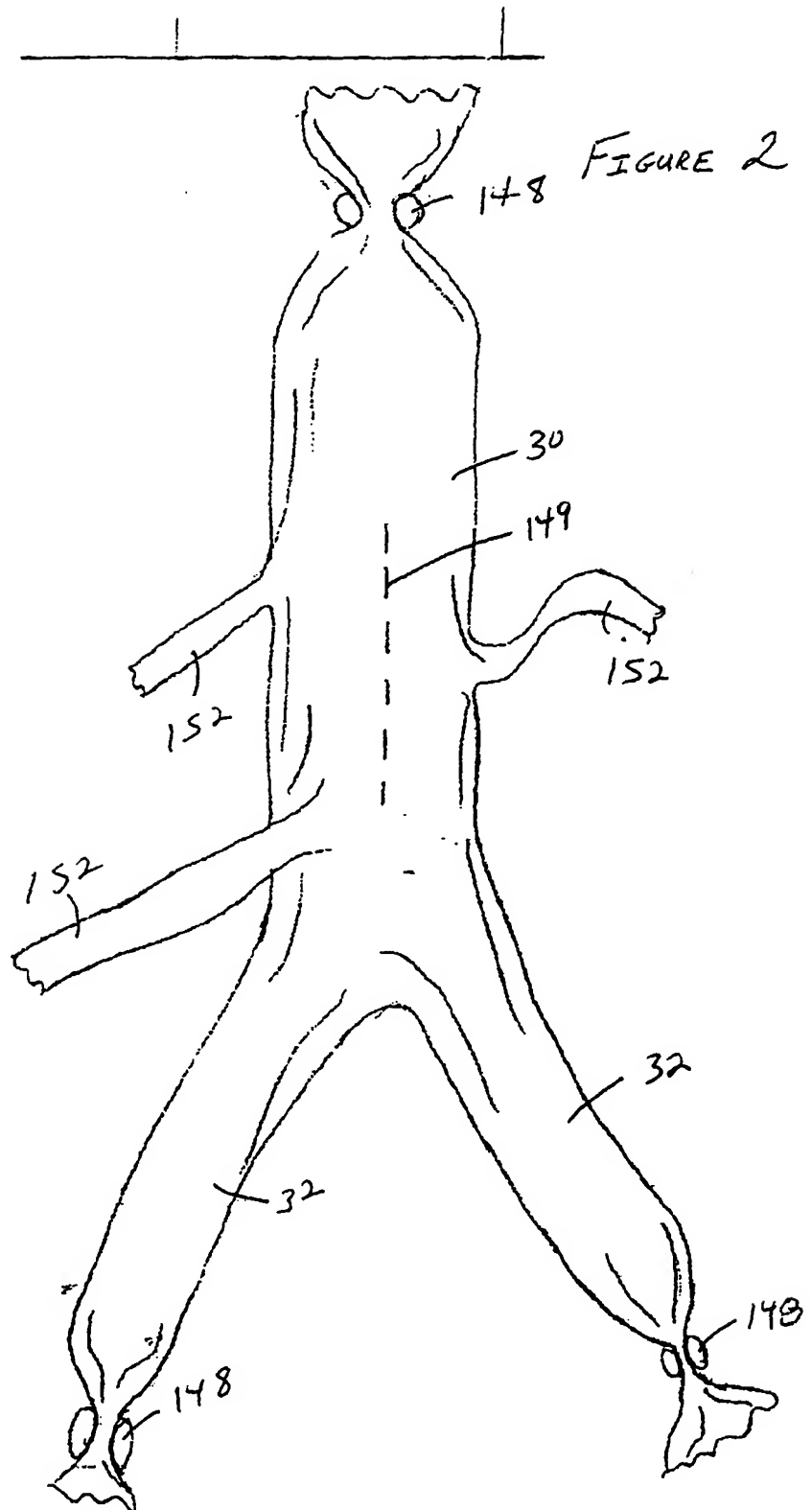
compress a vessel wall against their respective fittings at the two vessel

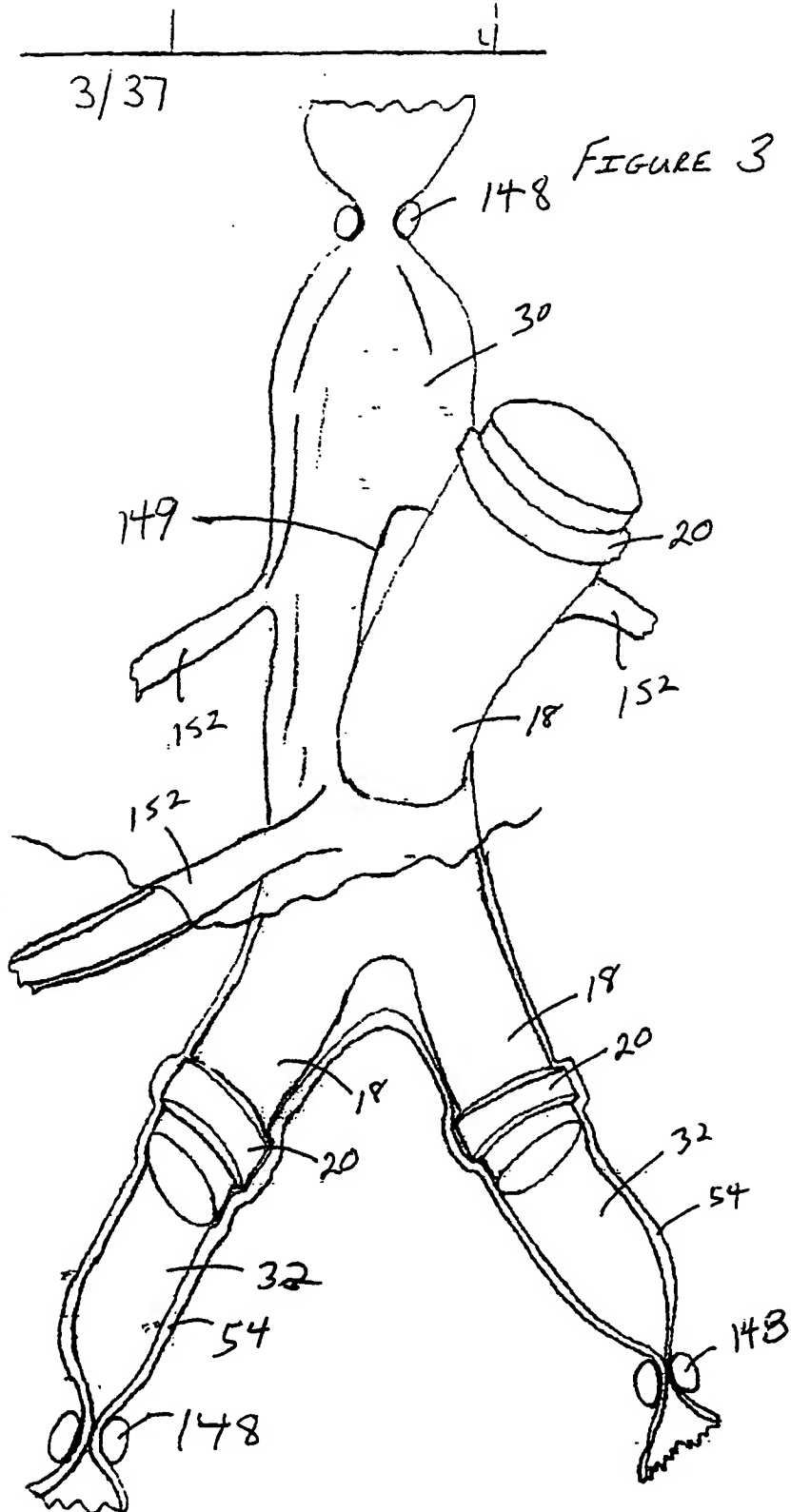
locations;

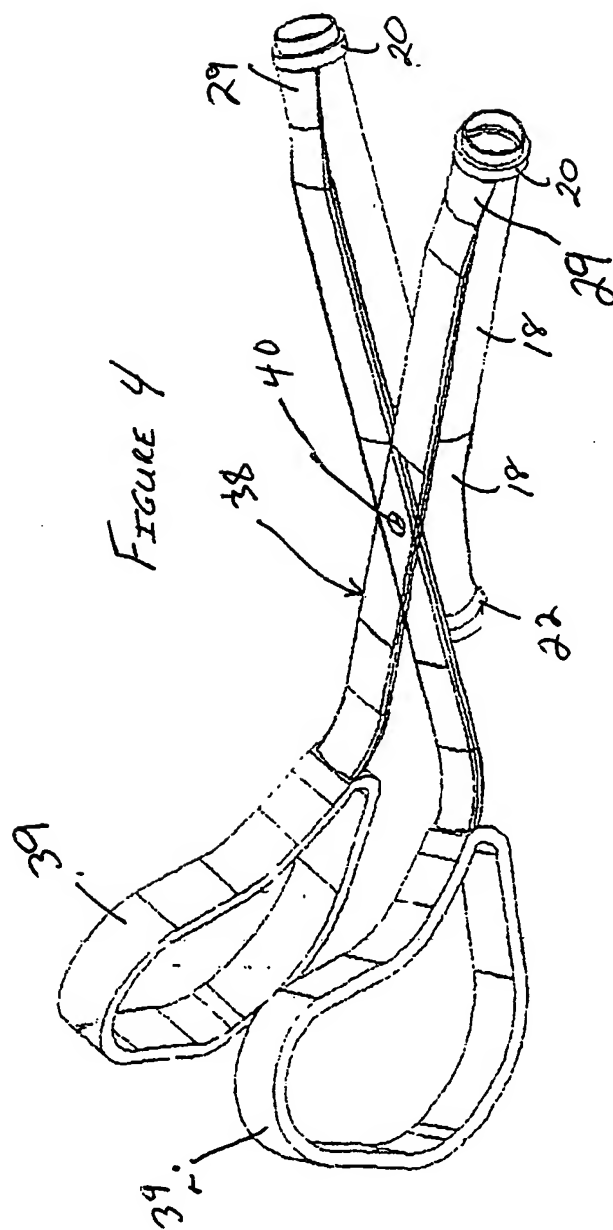
10 2. Devices and systems substantially as described herein.

FIGURE 1









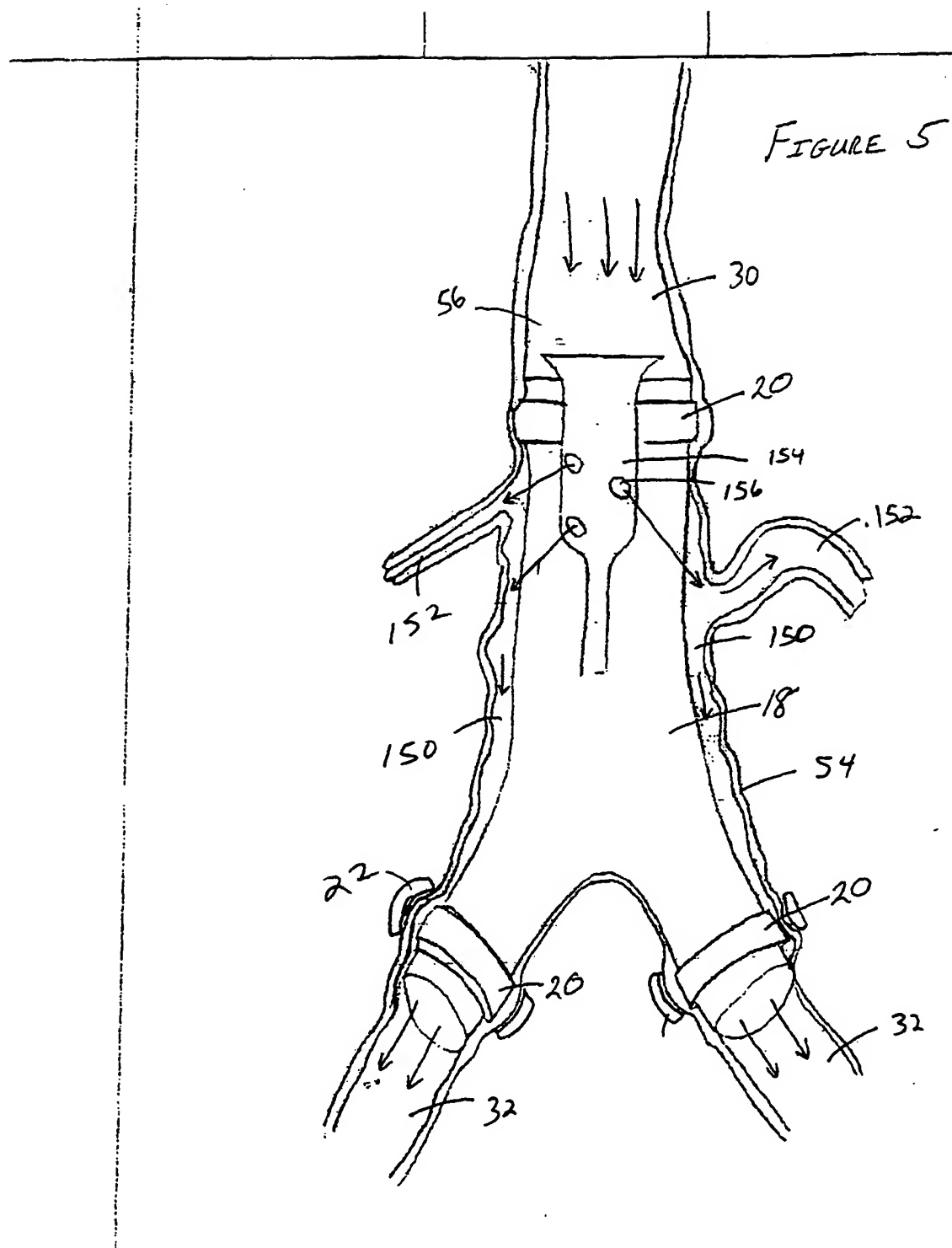


FIGURE 6a 154

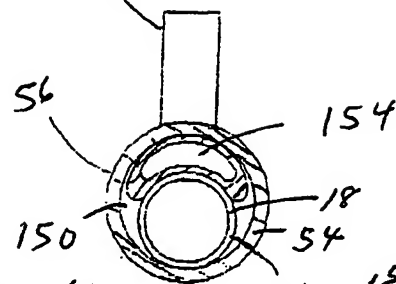
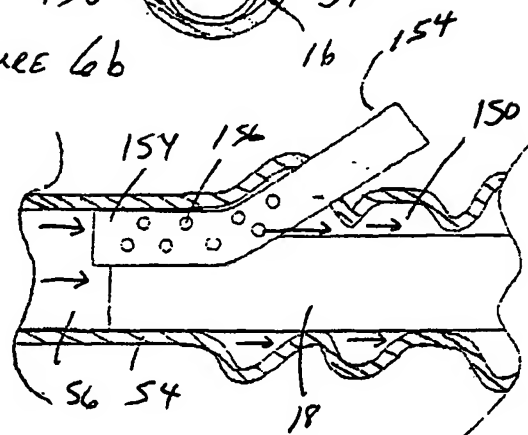


FIGURE 6b



7/37

FIGURE 7

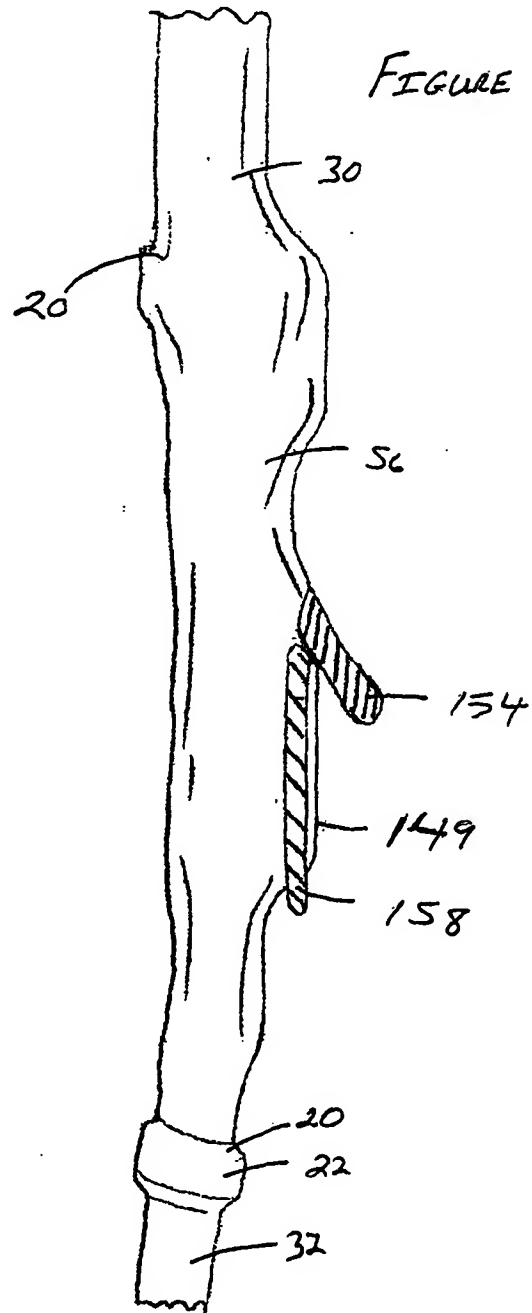
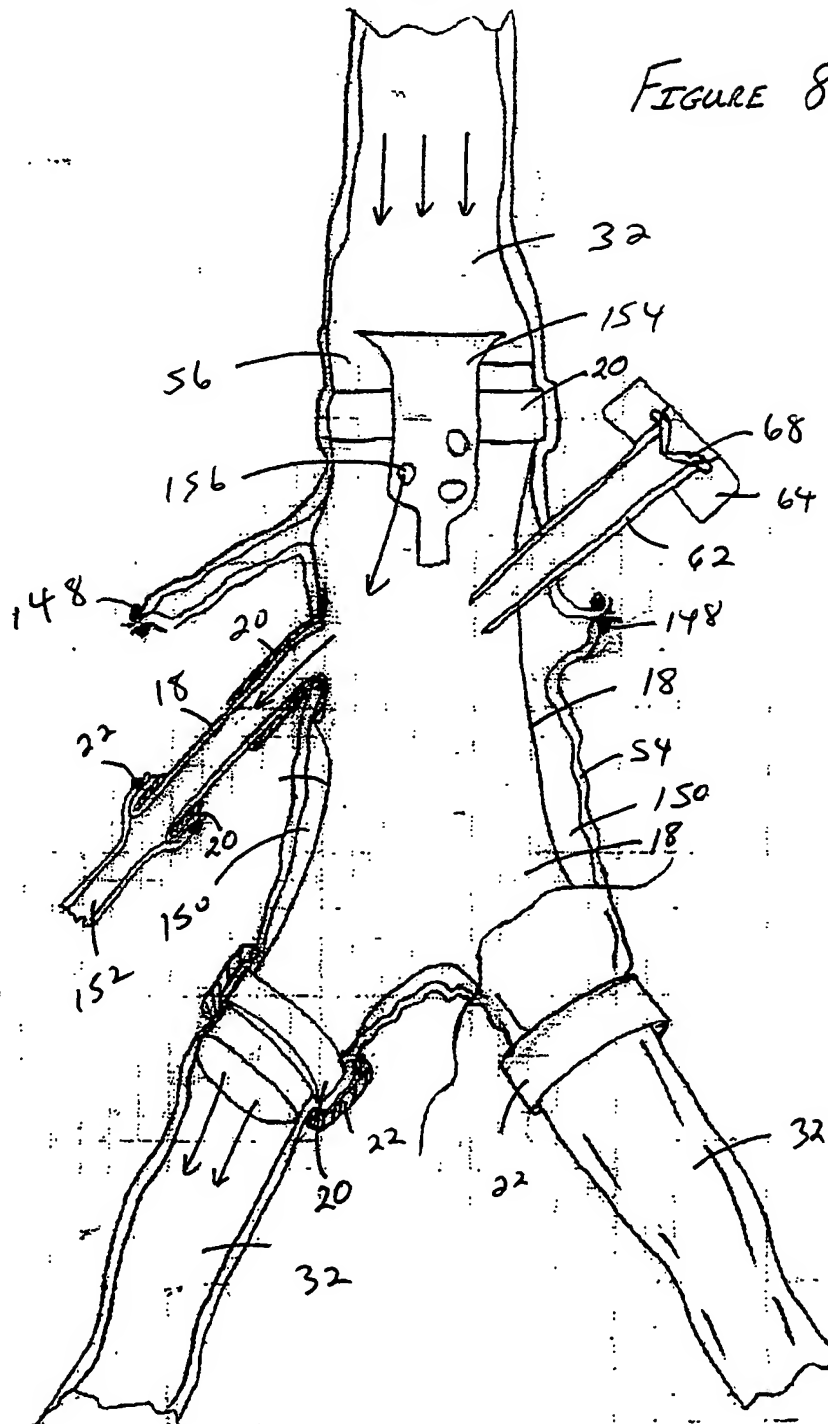
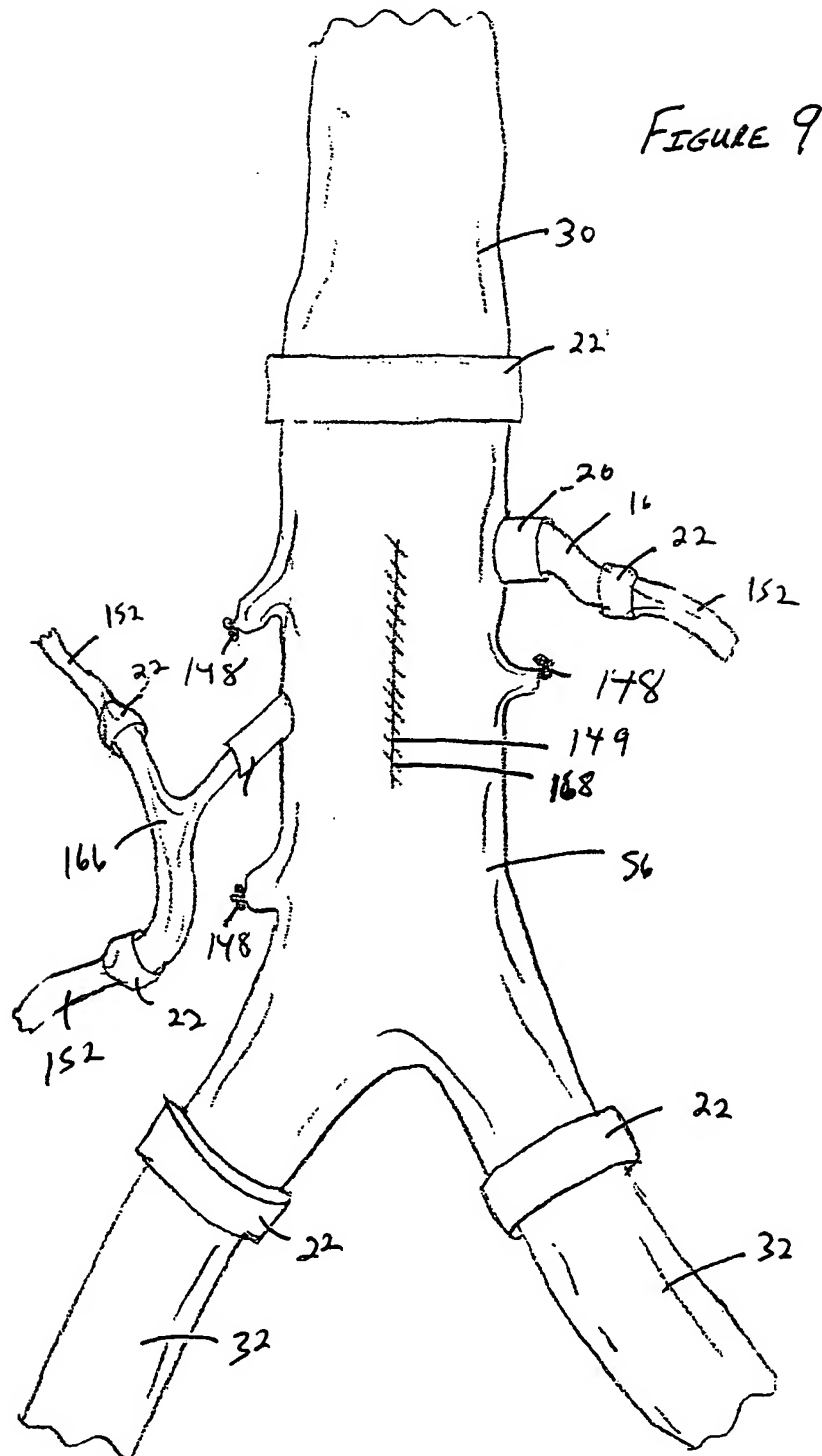
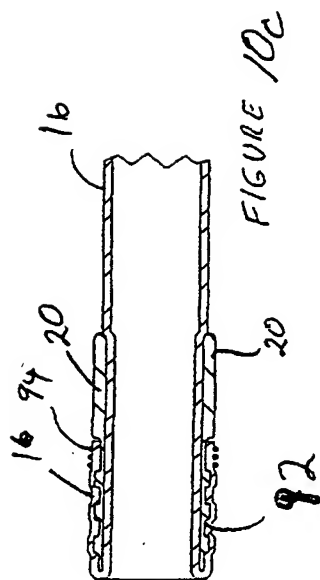
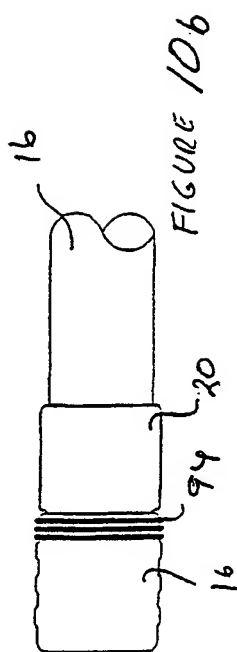
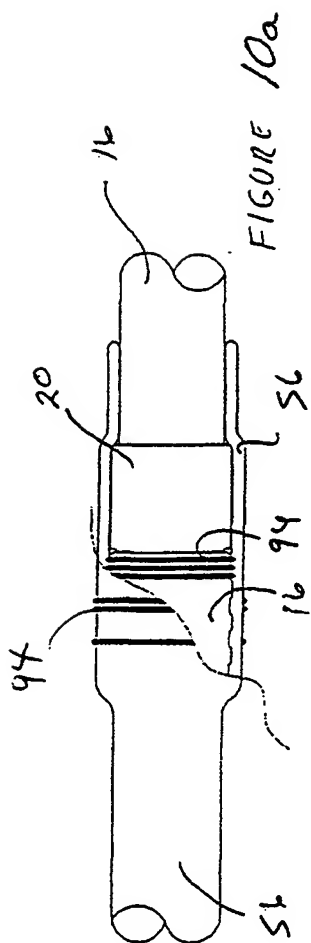
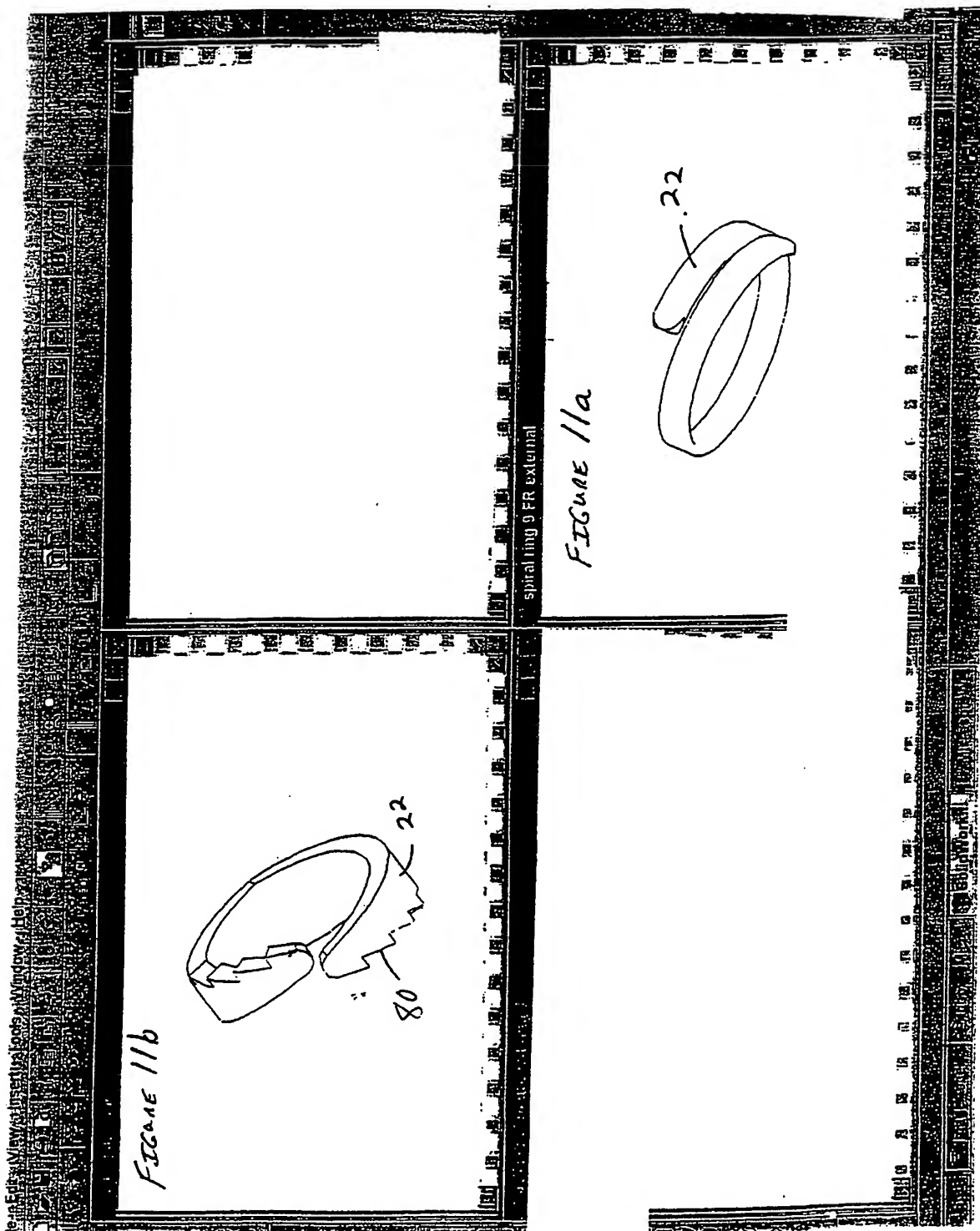


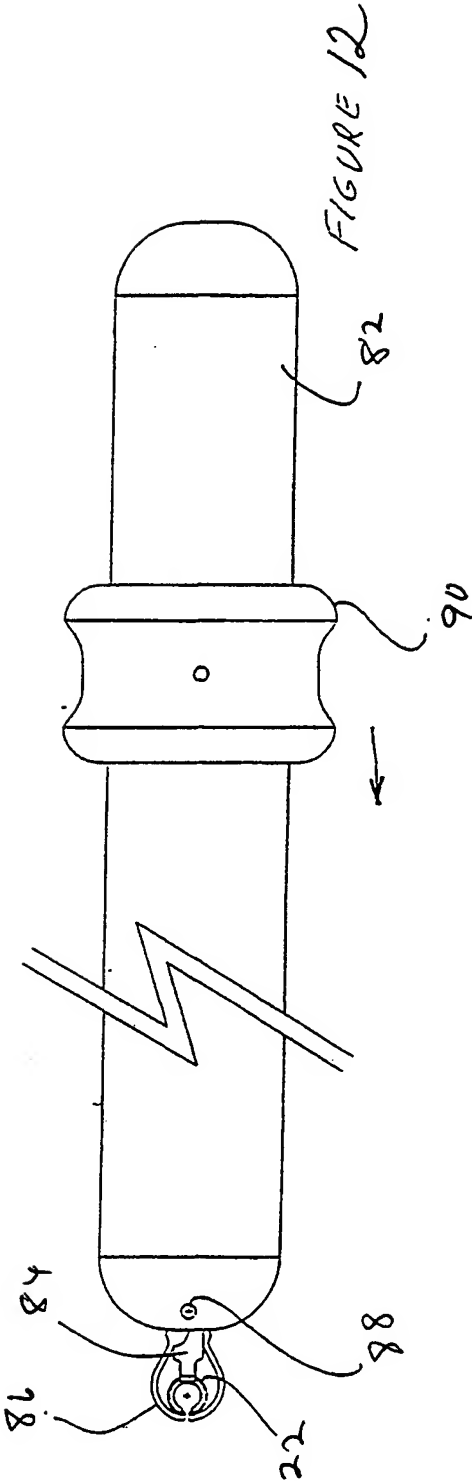
FIGURE 8

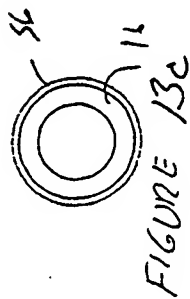
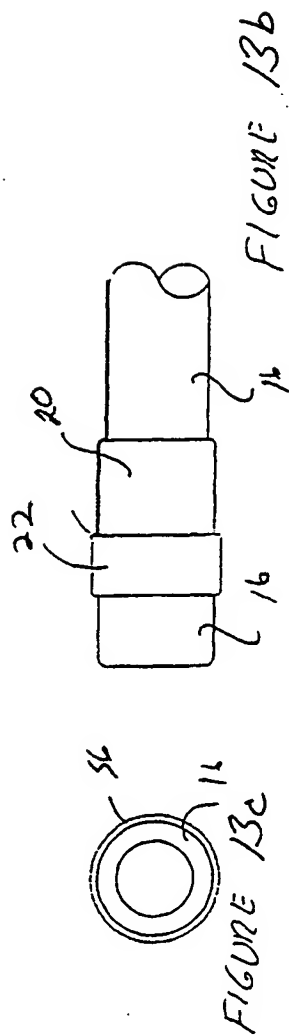
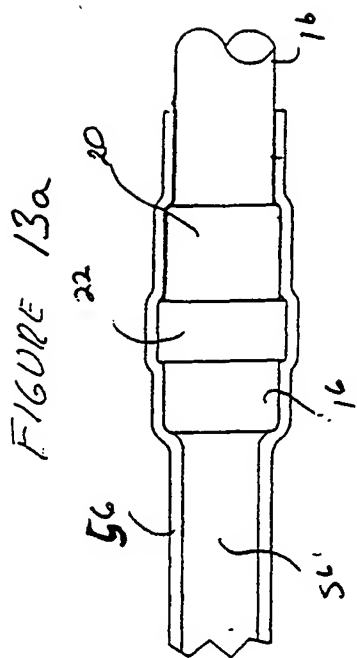


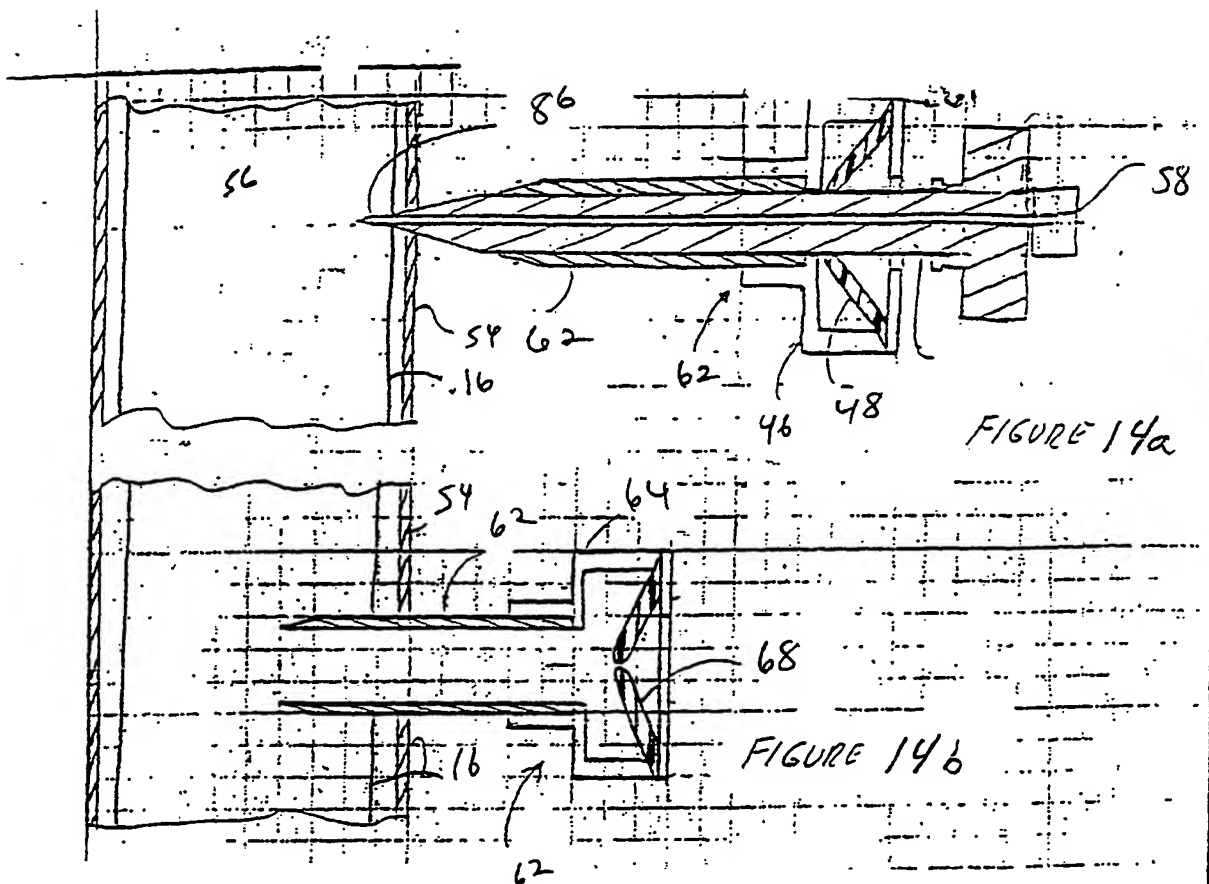


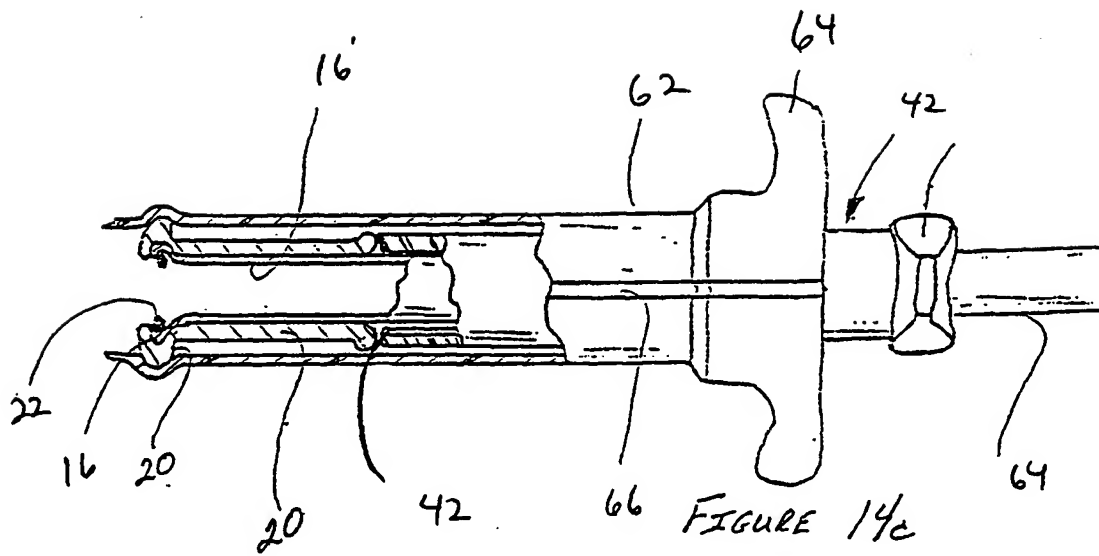


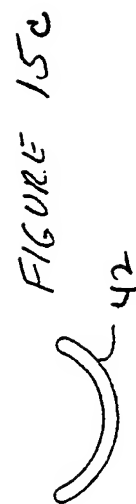
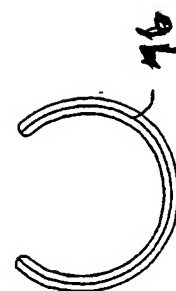
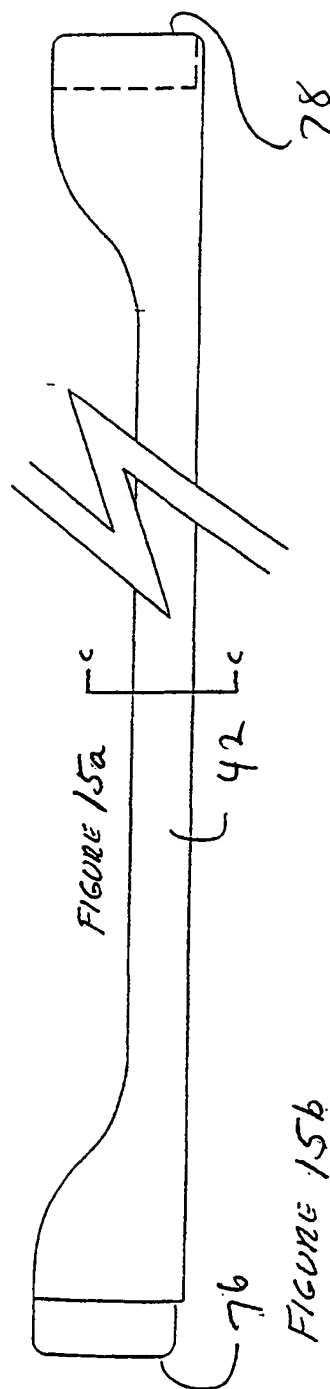












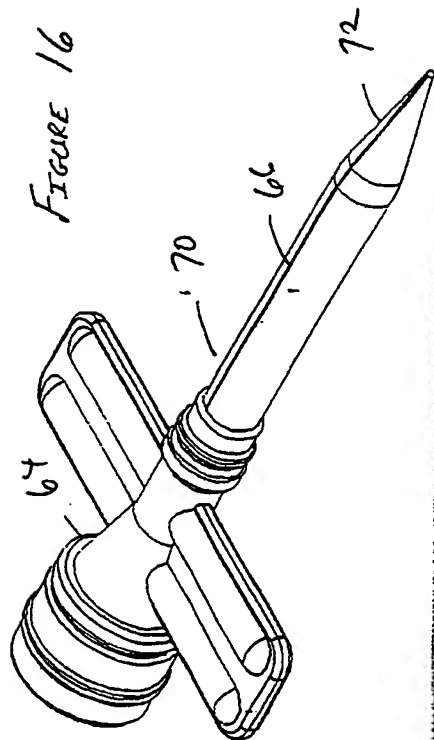


FIGURE 17a

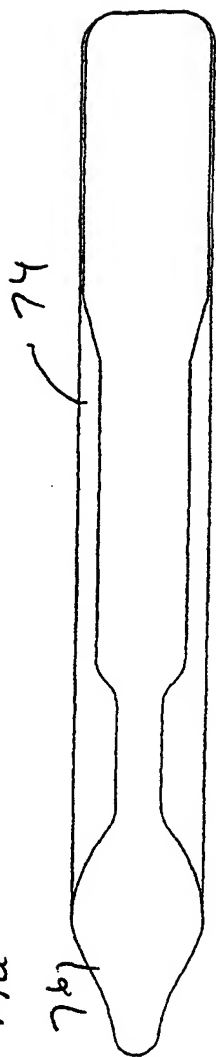


FIGURE 17b

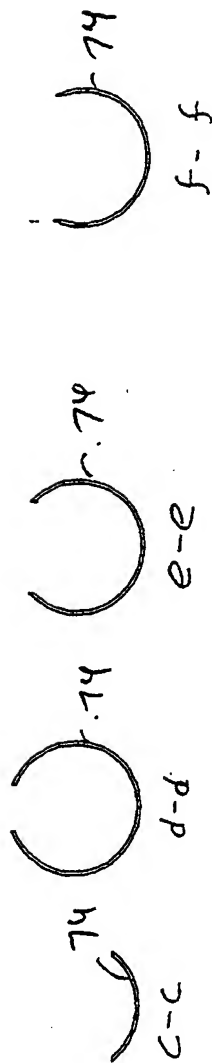
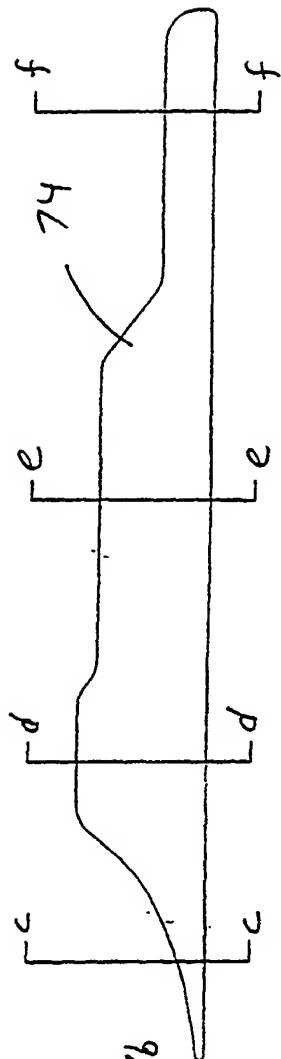


FIGURE 17c

FIGURE 17d

FIGURE 17e

FIGURE 17f

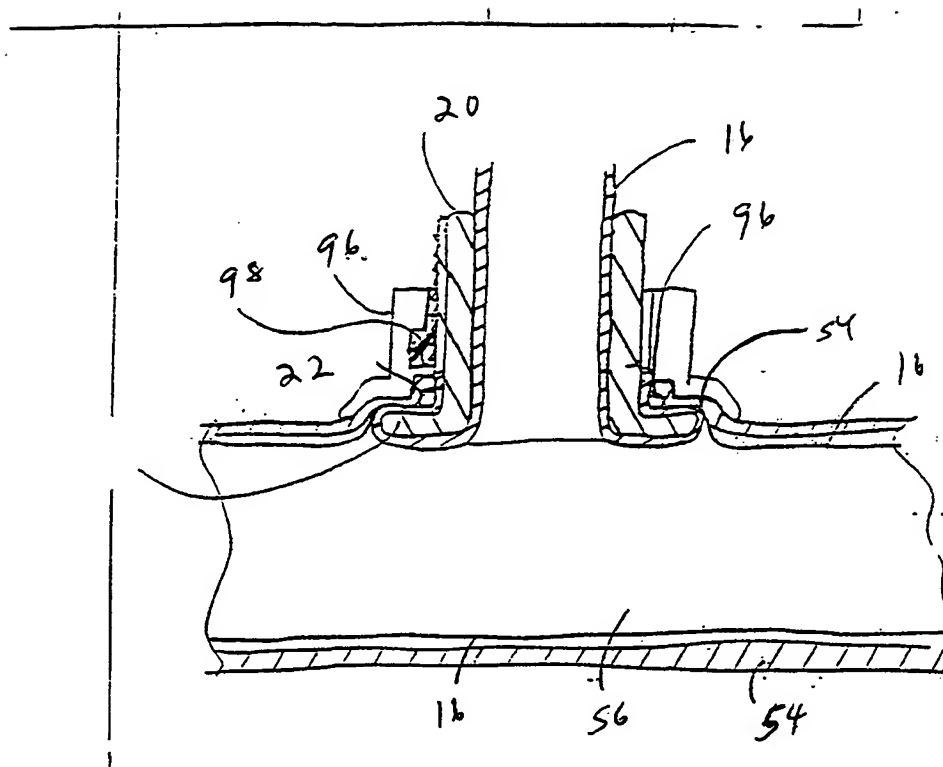


FIGURE 18

FIGURE 20b

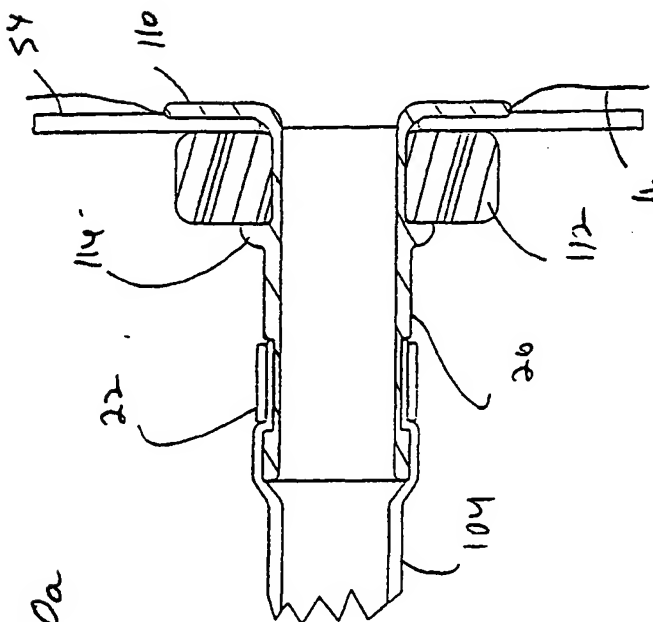
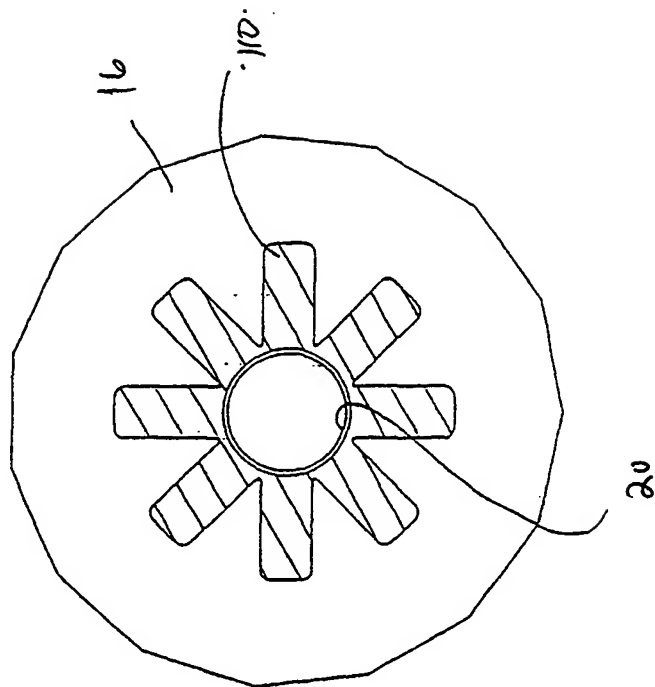


FIGURE 20a

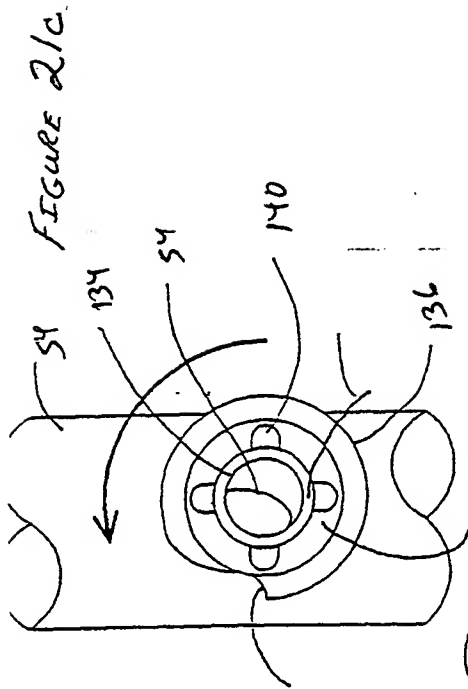


FIGURE 21b

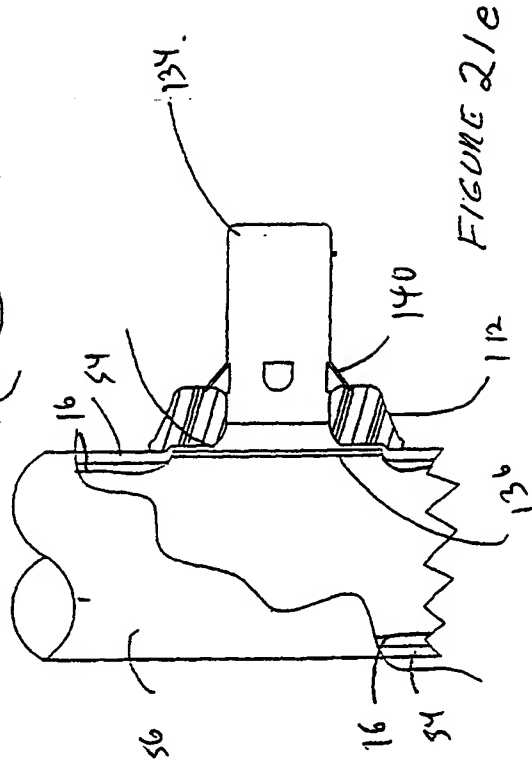
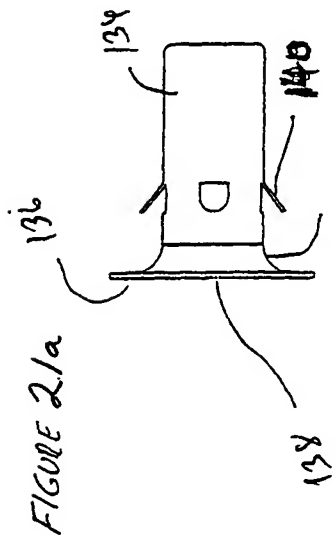
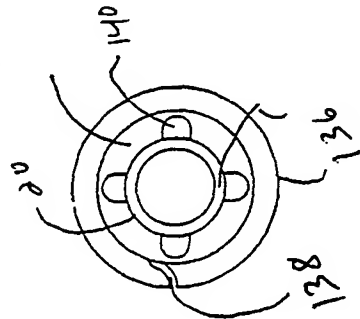


FIGURE 21e

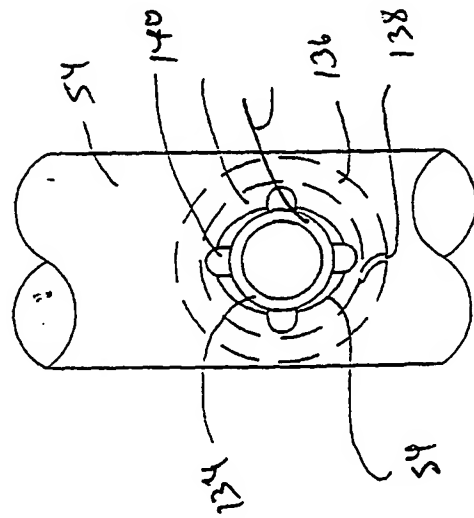
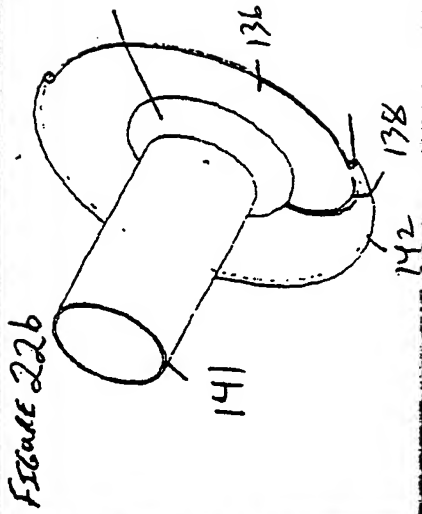
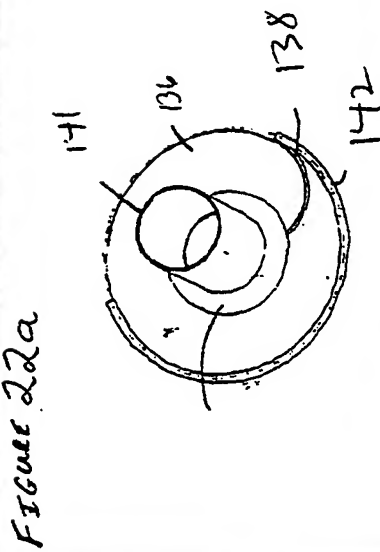
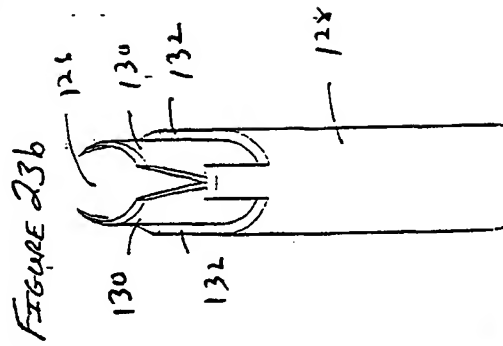
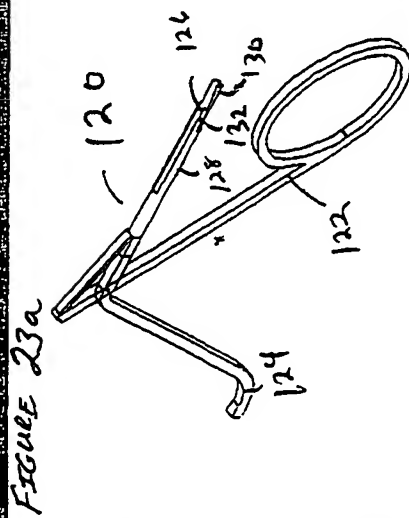
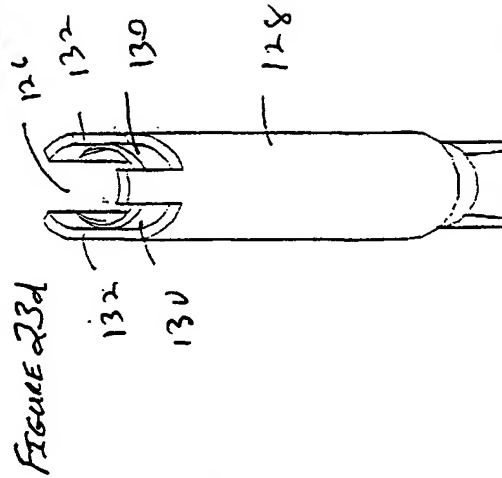
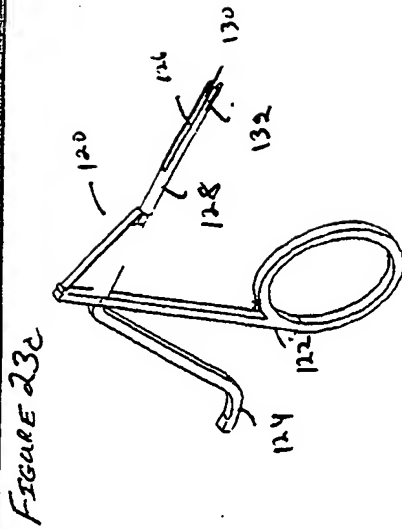
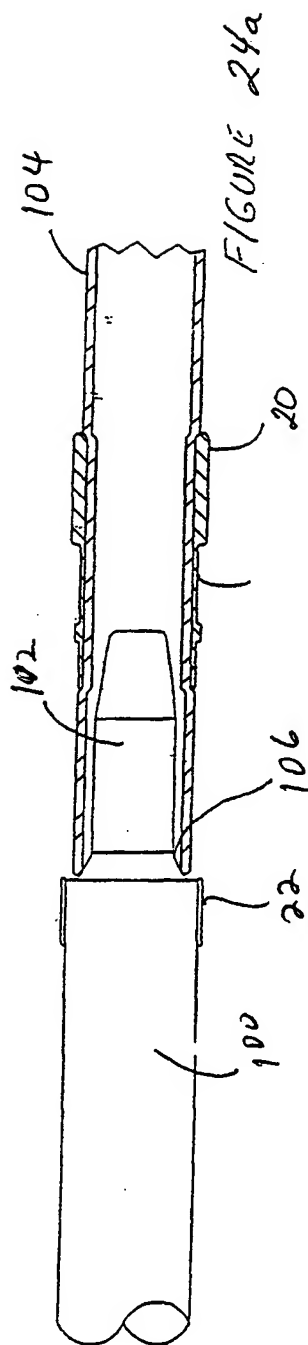
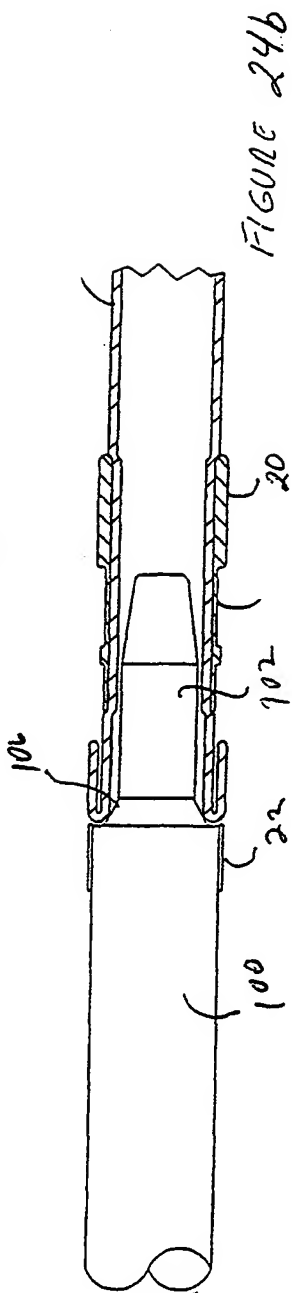
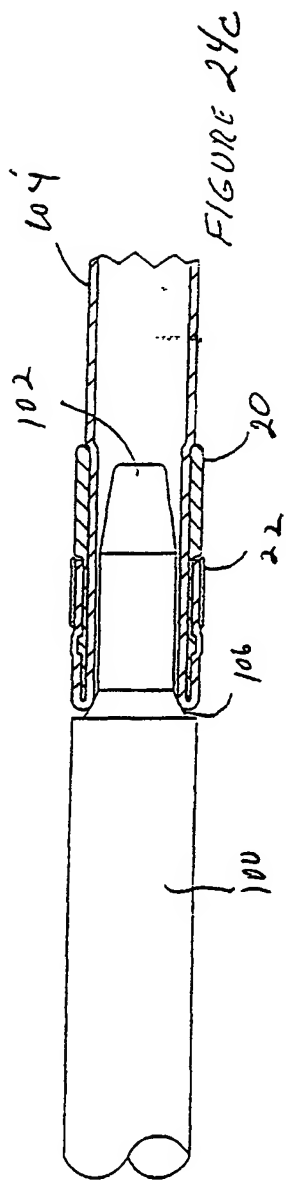


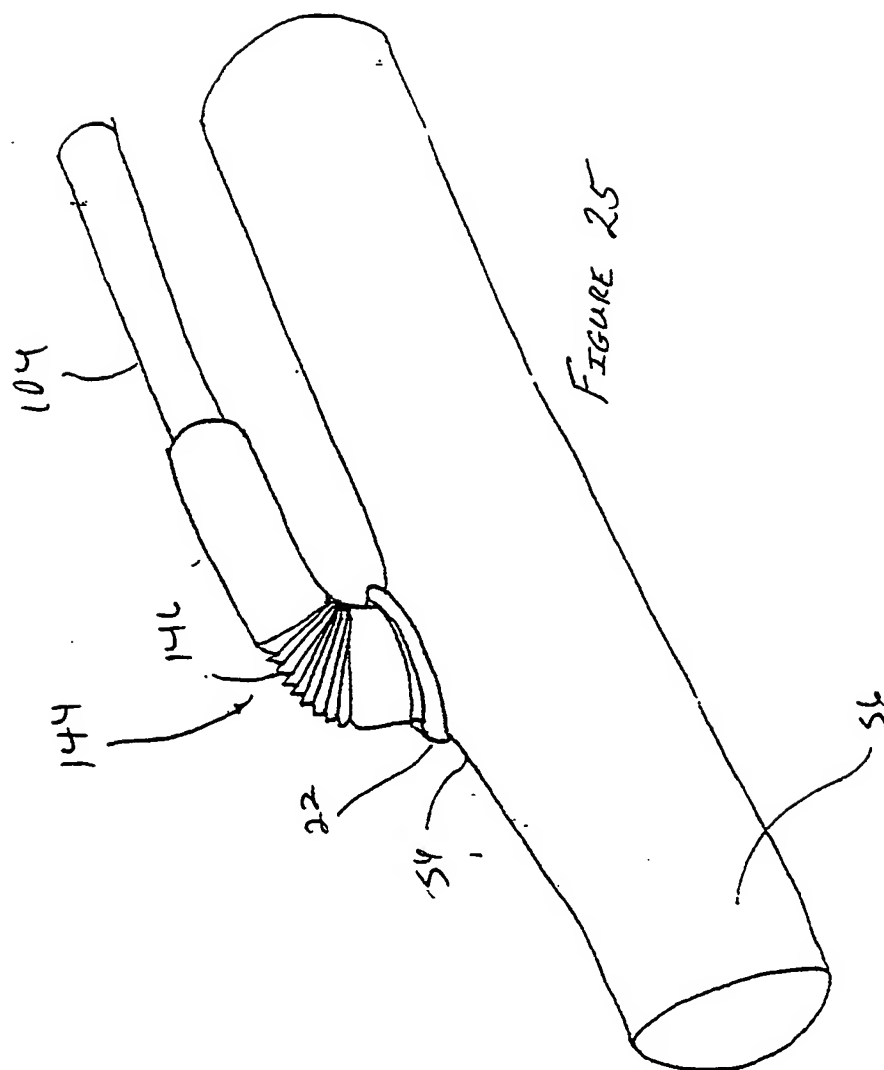
FIGURE 21d











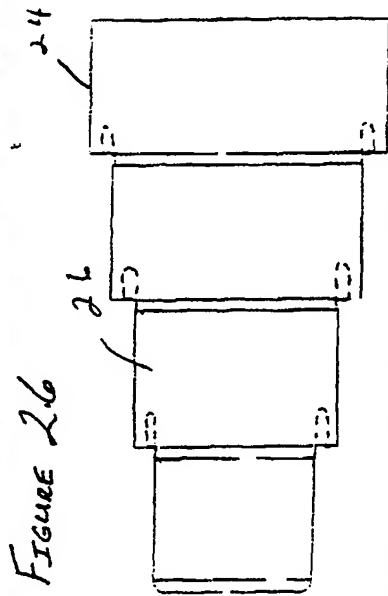


Figure 27

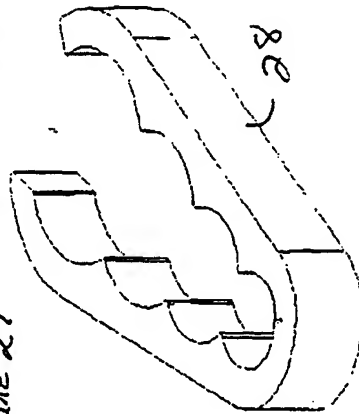
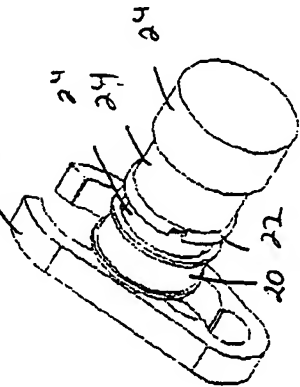
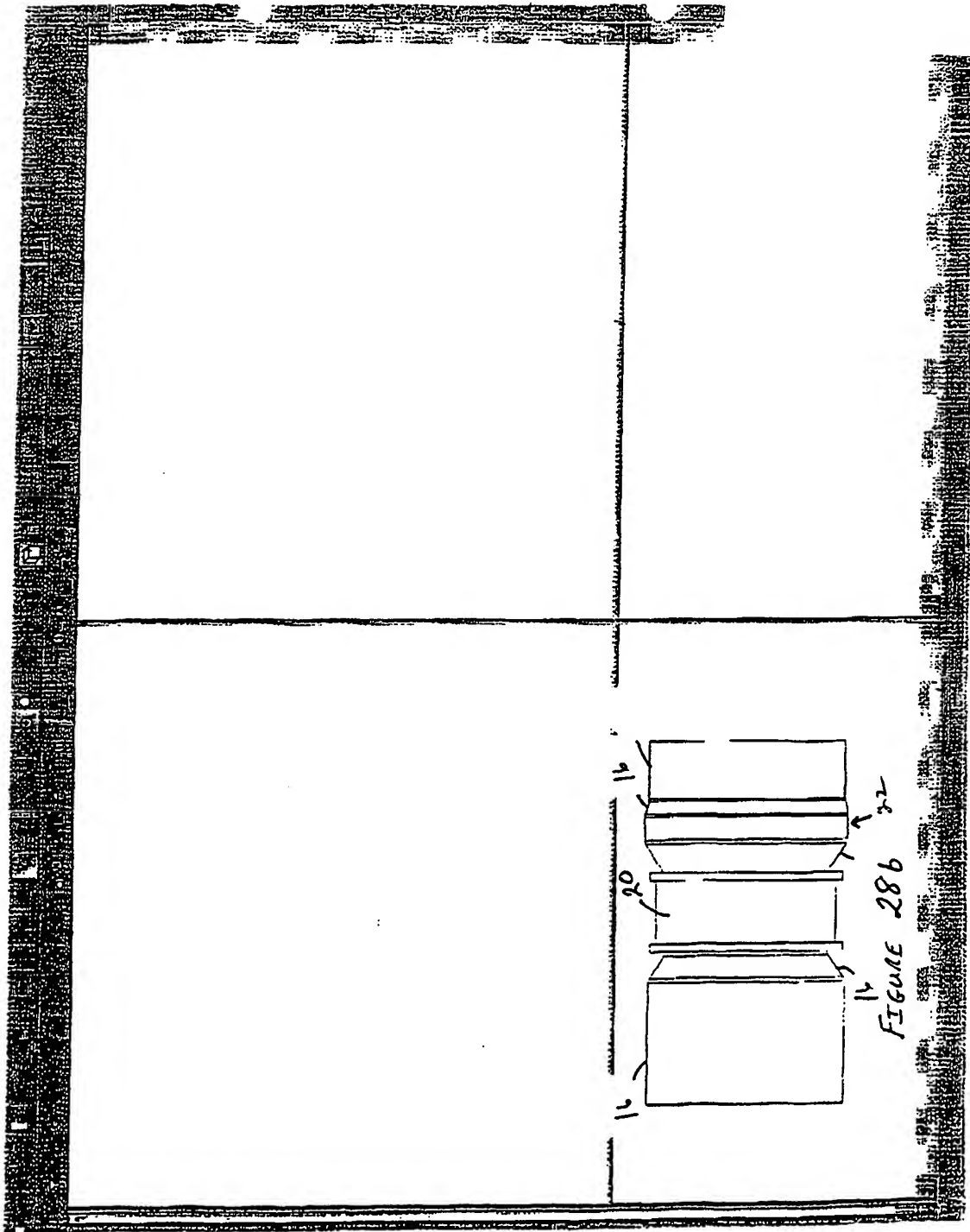
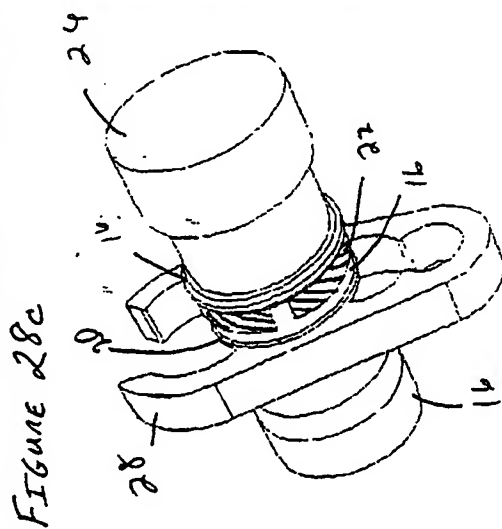


Figure 28a



Assem2AG
 Front
 Top
 Right
 Left
 Origin
 (-) Grass
 (-) Fillin
 (-) Inset
 (-) Ring
 Front
 Top
 Right
 Left
 Origin
 (-) Base
 (-) Boss
 (-) Annot
 (-) Base
 MateGr
 Annotat





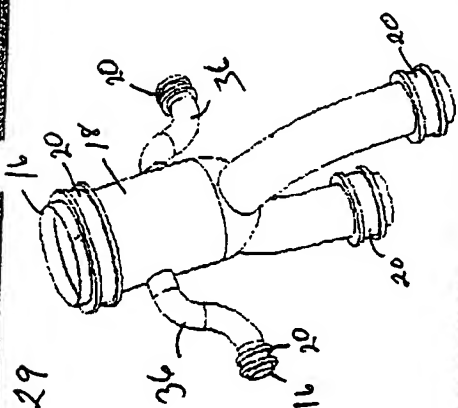


FIGURE 29

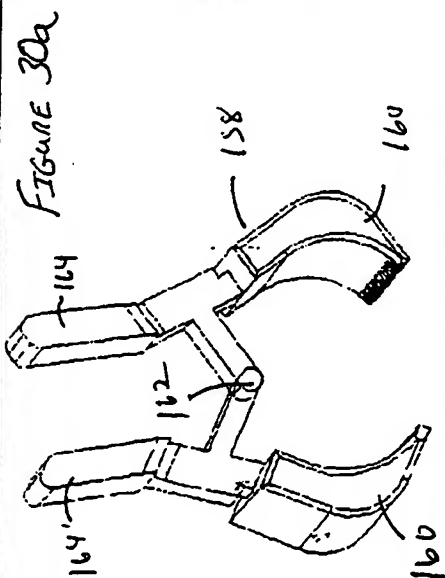
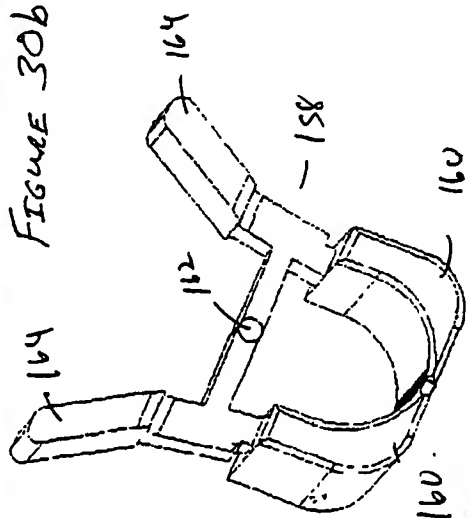
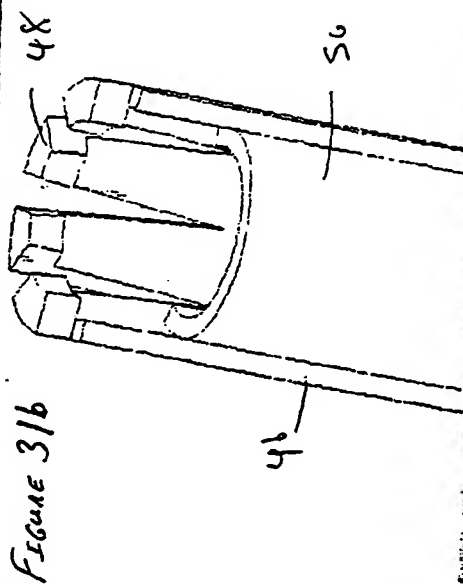
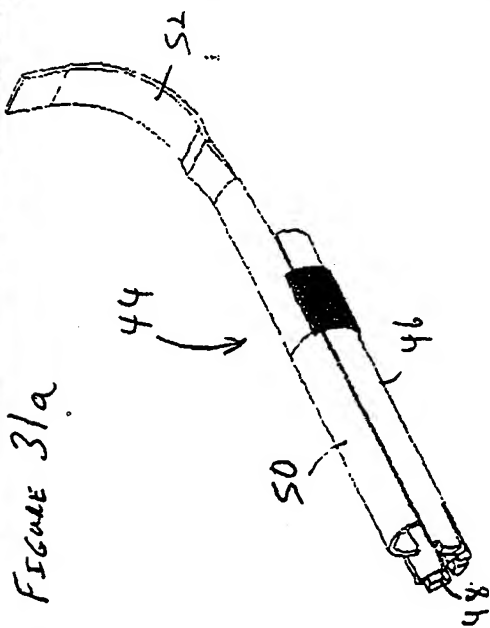


FIGURE 30b





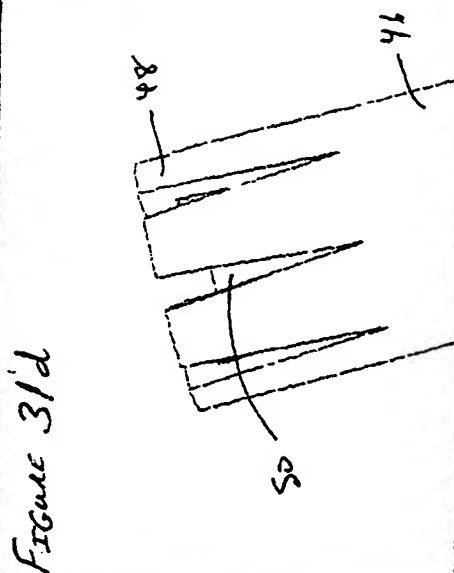
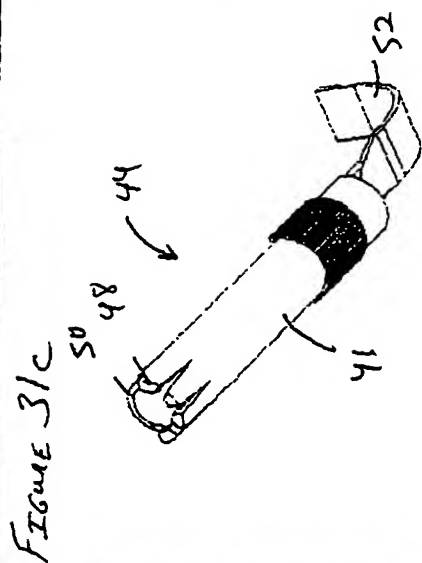


FIGURE 31e

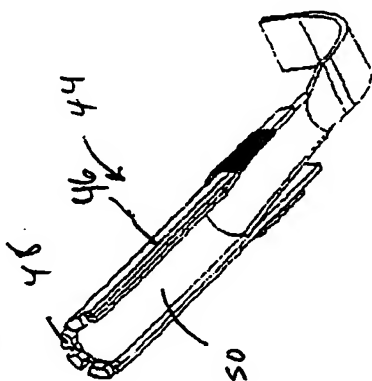
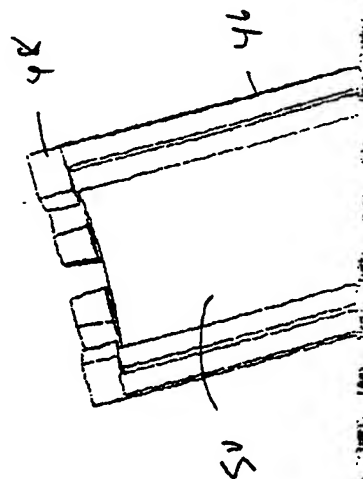


FIGURE 31f



INTERNATIONAL SEARCH REPORT

International application No

PCT/US99/13189

A. CLASSIFICATION OF SUBJECT MATTER

IPC(6) : A61F 2/06

US CL : 623/1

According to International Patent Classification (IPC) or to both national classification and IPC

B. FIELDS SEARCHED

Minimum documentation searched (classification system followed by classification symbols)

U.S. : 623/1

Documentation searched other than minimum documentation to the extent that such documents are included in the fields searched

Electronic data base consulted during the international search (name of data base and, where practicable, search terms used)

C. DOCUMENTS CONSIDERED TO BE RELEVANT

Category*	Citation of document, with indication, where appropriate, of the relevant passages	Relevant to claim No.
A	US 5,443,497 A (VENBRUX) 22 August 1995.	1, 2
A	US 5,405,322 A (LENNOX et al.) 11 April 1995.	1, 2
A	US 5,665,117 A (RHODES) 09 September 1997.	1, 2

☐ Further documents are listed in the continuation of Box C.
 ☐ See patent family annex.

* Special categories of cited documents:	"T" later document published after the international filing date or priority date and not in conflict with the application but cited to understand the principle or theory underlying the invention
"A" document defining the general state of the art which is not considered to be of particular relevance	"X" document of particular relevance; the claimed invention cannot be considered novel or cannot be considered to involve an inventive step when the document is taken alone
"E" earlier document published on or after the international filing date	"Y" document of particular relevance; the claimed invention cannot be considered to involve an inventive step when the document is combined with one or more other such documents, such combination being obvious to a person skilled in the art
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"P" document published prior to the international filing date but later than the priority date claimed	

Date of the actual completion of the international search

10 AUGUST 1999

Date of mailing of the international search report

20 OCT 1999

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